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Radiographic assessment of carpal conformation in the horse: Technique development and validation of the consistency of measurements

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Title: RADIOGRAPHIC ASSESSMENT OF CARPAL CONFORMATION IN THE HORSE: TECHNIQUE DEVELOPMENT AND VALIDATION OF THE CONSISTENCY OF MEASUREMENTS

Running head: OBJECTIVE EVALUATION OF THE EQUINE CARPUS

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1 **ABSTRACT**

2 Carpal conformation is often considered as a contributory factor to performance and lameness in the
3 horse; however, few attempts have been made to objectively measure radiographic variations of
4 carpal conformation in horses due to insufficient measurable carpal parameters. This pilot study used
5 carpal radiographic images acquired from 10 cadaveric equine forelimbs transected at the antebrachial
6 midshaft from 7 adult horses (7.2±2.6 years), positioned at “zero lateromedial” (ZLM) and “zero
7 dorsopalmar” (ZDP) views, to investigate the anatomy of the equine carpus and develop parameters
8 that could be objectively used to assess carpal conformation in horses.

9 Dorsal carpal angle (DCA: 176.61±0.66°), distal radial slope carpal angle (DRSCA: 145.59±2.19°),
10 intermediate carpal bone proximal tuberosity-radial angle (CiPxTRA: 115.69±3.15°) and third carpal
11 bone palmar facet angle (C3PalFCA: 84.43±1.13°) were all developed from the ZLM view while
12 medial carpal angle (MCA: 183.34±1.02°), disto-dorsal slope angle of the third carpal bone
13 (C3DDSA: 8.27±0.92°) and width ratio of distal radius to proximal metacarpus (WDR:WPM =
14 1.13±.03) were 3 of the 10 parameters developed from the ZDP view.

15 Easy to identify and measurable parameters will help to provide quantitative assessment of carpal
16 conformation in the horse with potential of eliminating subjective observational variation errors
17 between clinicians. These newly developed parameters will be useful in further studies to measure
18 variations in the conformation of the equine carpus in live horses and comparison between subjective
19 visual assessment and objective radiographic evaluation methods.

20 **Key words:** Carpal conformation; Carpal joint; Horses; Measurable parameters; Radiographs; Equine

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28 **1. INTRODUCTION**

29 The conformation of the equine forelimb is very important to the overall athletic performance
30 of the horse and its susceptibility to lameness as it bears over 55% of the horse’s standing weight and
31 is subjected to high compressional forces during galloping and landing phase of jumping (Clayton *et*
32 *al.*, 2013; Kainer, 2002). The carpus must transmit large axial loads from the antebrachium to the
33 distal forelimb and maintain optimum structural stability if the horse is to meet the heavy demand of

1 training, racing, and other athletic performances (Stashak & Hill, 2002). This stability is largely
2 dependent on the conformation of the carpal bony structures.

3 Although some radiographic parameters have previously been developed to assess carpal
4 conformation in horses; only few parameters are however regularly utilized. These include measuring
5 “carpal angle” from both the dorsopalmar (DPa) and lateromedial (LM) radiographs (Barr, 1994;
6 Fretz 1980); which the current authors have termed “medial carpal angle (MCA) and dorsal carpal
7 angle (DCA) respectively to eliminate confusion in their description and orientation. In 2011,
8 Abdunnabi developed 37 parameters from DPa radiographs and proposed their use in the
9 conformational assessment of the equine carpus (Abdunnabi, 2011; Oheida *et al.*, 2016). Although, in
10 contrast to previous studies (Barr, 1994; Fretz 1980), Abdunnabi (2011) validated the repeatability
11 and reproducibility of specific landmarks used in developing the 37 DPa parameters, however the
12 complexity involved in measuring most of these 37 parameters might make them unsuitable for
13 routine/practical use. These complexities added to the shortcomings of objective carpal evaluation and
14 may partly explained why only 10 out of the 37 parameters were published (Oheida *et al.*, 2016).

15 The equine carpal bones are classified as short bones (Getty, 1975) and have also been
16 described as wedge-like in shape with topographic angulation of their articular surfaces (Bramlage,
17 1988; Deane & Davies, 1995a; Kainer, 2002; Von Rubeli, 1925). The carpal bones slide into a “close
18 packed position” during weight bearing (a position where full congruities of all opposite and adjacent
19 articular surfaces of the carpal bones occurred) and this unique morphology is believed to assist the
20 carpus in attenuation of large axial forces by transferring some strain into the elastic intercarpal
21 ligaments (Bramlage, 1988; Deane & Davies, 1995a; Von Boening, 1981). None of the 37 parameters
22 (Abdunnabi, 2011; Oheida *et al.*, 2016) fully considered the topography of the articular surfaces of the
23 carpal bones. Further investigation of the anatomy of the carpal DPa radiographs might therefore
24 produce more measurable parameters that could estimate the degree of wedge or steepness of slope of
25 these articular surfaces.

26 It would be beneficial to develop parameters from both the dorsopalmar and lateromedial
27 radiographs of the carpal joint that would measure both the morphological and alignment aspects of
28 conformation. This would provide a more holistic assessment of the carpal conformation in horses and
29 probable predictive indices for biomechanical function and pathology of carpal joints. These
30 parameters should be easy to measure, have consistent landmarks, reliably measure carpal
31 conformational features, and show good repeatability (reliability) and reproducibility within and
32 between different observers. Intraclass correlation coefficient (ICC) measures the reliability or
33 consistency of measurements between two or more observers and could also show the reproducibility
34 of experimental method and or agreement between two or more repeated measurements and observers
35 (Bobak *et al.*, 2018; Koo & Li 2016; Liljequist *et al.*, 2019). The aims of this pilot study were: i) to
36 investigate the radiographic anatomy of the equine carpus and develop measurable parameters such as
37 angles and ratios that could be used to objectively measure the conformation of the carpus, ii) to

1 describe a detailed radiographic method for the measurement of the identified parameters, iii) to
2 investigate the consistency of the positions of landmarks used to establish these parameters and iv) to
3 investigate the reliability of the measurement protocol (parameters) between observers.

4 **2. MATERIALS AND METHODS**

5 **2.1. Development of radiographic measurement techniques**

6 **Study design:** This was a pilot study designed to test measurement and data collection protocol.

7 **Ethical animal research:** Approval from the University of Melbourne Animal Ethics Committee was
8 not required as specimen were collected from animals that had either died or were euthanized for
9 reasons not related to the study.

10 **Animals:** 10 forelimbs (from 7 thoroughbreds) aged 7.2 ± 2.6 years were collected from the post-
11 mortem room of the Department of Veterinary Pathology, University of Melbourne, Australia, and a
12 local knackery in Melbourne. All the horses had either died or were euthanized for conditions not
13 related to carpal injuries or lameness and owners' consent to use cadavers was obtained. The limbs
14 were transected at about the midshaft of the antebrachium, wrapped in plastic bags, and preserved by
15 freezing at -20°C until needed. Only limbs with carpi that had no visible physical injury and no
16 radiographic abnormalities were included in the study.

17 **Limb preparation and radiography:** The limbs were defrosted in a chiller (5°C) for about 72 hours.
18 Thereafter, each limb was mounted in a standing position on a customised loading rig (Alrtib, 2013)
19 (Figure 1) and radiographed through lateromedial and dorsopalmar views using a portable
20 radiographic machine (Atomscope HF80/15 UltraLight, Mikasa X-ray Co Ltd, Japan) set at 80 KVp
21 and 24 secs (3.6 mAs). A common practice in our research group: Functional Anatomy and
22 Biomechanics Laboratory (FABLAB), University of Melbourne, adopted for equine field radiography
23 is to acquire images of the left limb in the lateromedial view and the right limb in the mediolateral
24 position. This minimizes disturbance to the horses and reduces operational time per animal. A set of
25 two lateral radiographs (i.e. lateromedial and mediolateral views) were therefore acquired for each of
26 the 10 cadaveric limbs for comparison of carpal measurements on both lateral images.

27 **2.1.1. Zero lateromedial/mediolateral (ZLM/ZML) carpal image**

28 A specific rotational (oblique) image of the lateromedial view of the carpus, where the second and
29 fourth metacarpal bones completely overlap, was acquired by slightly rotating the limb until the
30 desired image was produced. This specific carpal image was defined as the "zero lateromedial"
31 (ZLM) image (Figure 2a) produced from a "zero lateromedial" (ZLM) view or position. All carpal
32 parameters were thereafter developed, measured, and compared on both zero lateromedial "ZLM" and
33 zero mediolateral "ZML" images/views.

34 **2.1.2. Zero dorsopalmar (ZDP) carpal View/image**

35 The zero dorsopalmar (ZDP) view or image was defined as a dorsopalmar (DPa) view of the carpus at
36 which its rotations along the vertical and horizontal axes were at zero degrees (Figure 2b)

1 (Abdunnabi, 2011; Oheida *et al.*, 2016). A straight line drawn to represent the proximal edge of the
2 metacarpus and referred to as the reference line (RL) was previously established by Abdunnabi (2011)
3 and reported to be parallel with the ground (Abdunnabi, 2011; Oheida *et al.*, 2016). These 2
4 previously established specific profiles of the DPa view (i.e ZDP and RL) were adopted for this study
5 (Figure 2b).

6 The wedge angles of intermediate carpal bone (Ci) and the fourth carpal bone (C4) were
7 measured directly from the radiographs while the slopes of the articular facets of the third (C3), radial
8 (Cr) and ulnar (Cu) carpal bones were respectively used to calculate the respective slope angles for
9 the C3, Cr and Cu. Geometrically, a wedge is a type of polyhedron (triangular prism) usually defined
10 by two right angle triangles and three trapezoid faces. Using the principle of the right-angle triangle to
11 relate to the “wedge-like” morphology of the carpal bones, if a long enough line (slope line) is drawn
12 from the point of the wedge slope of each carpal bone facet (e.g. Cr and C3), it will eventually meet
13 the continuation of the RL, and the angle thus formed would be termed the slope angle (x°) of that
14 particular carpal bone facet (Figure 3). Another line drawn perpendicularly from any position on the
15 RL to meet the wedge slope line will form another angle (y°). If angle y° was measured and then
16 added to the known constant (90°) of right-angle triangles; then, the summation of y° and 90° could
17 then be subtracted from 180° to get x° [i.e. $x = 180 - (90+y)$]. A parallel line to the RL on any
18 transverse plane could be drawn to form the base of the right-angle triangle for each carpal bone
19 wedge angle as required.

20 **2.2. Radiographic measurement of carpal parameters**

21 Selection of radiographs and development of measuring parameters (angles and ratios) were carried
22 out by observer 1. Measurement and data recording were carried out on separate occasions by
23 observer 1 and 2 at intervals of not less than 2 weeks from each set of measurements. All radiographic
24 images were processed by Veterinary-80 CR Scanner (3D Imaging & Simulations Corp., Yuseong-
25 Gu, Daejeon, Korea). Images were stored, analysed, and measured with an X-ray acquisition software
26 (DICOM PACS® DX-R). All measurements were carried out with the same computer hardware (Dell®
27 Latitude E6530). A summary of the abbreviations and meaning of some used technical details are
28 provided in table 5 (the appendix). The following carpal parameters were developed to measure
29 different aspects of carpal conformation.

30 **2.2.1. Carpal parameters measurable on zero lateromedial/mediolateral**

31 **(ZLM/ZML) radiographs**

32 **i. Dorsal carpal angle (DCA):** was defined as the angle formed dorsally at the intersection of the
33 long axis of the antebrachium and that of the third metacarpal bone. Although this angle was
34 previously measured by Barr (1994), it was first termed/named DCA by Olusa (2018) and Olusa *et*
35 *al.*, (2019). As shown in Figure 4a, the (dorsopalmar widths) of both the antebrachium and the
36 metacarpus were each measured at 60mm and 120mm from the antebrachiocarpal and

1 carpometacarpal joints respectively and marked at the middle (midpoint) of these width. A straight
2 line was then drawn through these marked midpoints of the bones to represent the long axis of both
3 the antebrachium and the third metacarpus

4 **ii. Distal radial slope carpal angle (DRSCA):** was defined (Olusa, 2018; Olusa *et al.*, 2019) as the
5 correlated angle formed by the disto-dorsal slope of the antebrachium as it articulates with the
6 proximal row of the carpal bones (Figure 4b: ABD). Line “AB” was drawn as best fit from the most
7 dorsal point of the rim of the distal radius through the distal epiphyseal slope of the radius, while line
8 “BD” represented the dorsal height of Ci; from the distodorsal end (D) to its proximodorsal end (B).

9 **iii. Intermediate carpal bone proximal tuberosity-radial angle (CiPxTRA):** was measured as the
10 angle formed from the highest point of the proximal articular surface (tuberosity) of Ci to the dorsal
11 radial alignment (Figure 4b: ABC) (Olusa, 2018; Olusa *et al.*, 2019).

12 **iv. Third carpal bone palmer facet angle (C3PalFCA):** was measured as the angle formed between
13 an extended line from the highest point of the proximal palmar articular surface of C3 (point E on
14 Figure 4) to the disto-dorsal edge of the proximal carpal row alignment and a line (DB) representing
15 the dorsal height of Ci (Figure 4b: EDB) (Olusa, 2018; Olusa *et al.*, 2019).

16 **2.2.2. Carpal parameters measurable on zero dorsopalmar (ZDP) radiographs**

17 **i. Medial carpal angle (MCA):** was the angle formed medially at the intersection of two lines drawn
18 to represent the long axes of the radius and third metacarpal bones (Figure 4c) (Olusa, 2018; Olusa *et*
19 *al.*, 2019).

20 **ii. Disto-dorsal slope angle of the third carpal bone (C3DDSA):** was the angle formed between the
21 RL and the distal edge of C3 (Figure 5a: FEI). A line representing the distal edge of C3 (FE) was
22 drawn from the most lateral end of the distal edge of C3 through to its most medial point and extended
23 to meet the RL to form the slope angle (“x”). A second line was drawn perpendicularly from the RL
24 to meet the line representing the distal edge of C3 (i.e FE) and the angle formed y° was measured and
25 added to the constant 90° and then subtracted from 180° to get x° .

26 **iii. Disto-dorsal slope angle of the radial carpal bone (CrDDSA):** This was the angle formed
27 between the RL and the dorsal aspect (slope) of the distal surface of Cr (Figure 5a: CD and Figure
28 5ai). A line “CD” drawn from the lateral margin of the disto-dorsal border of Cr (i.e the articulation
29 point of Cr with C1 and C3), through to its medial edge and extended long enough until it meet the
30 continuation of the RL represented the angle of the dorsal slope of the distal surface of Cr and was
31 denoted by “x” (as shown in Figure 3). A perpendicular line from the RL was drawn to meet this
32 distal slope line of Cr close to its lateral end to form the angle “y”. The summation of “y” and 90°
33 when subtracted from 180° produced “x”.

34 **iv. Proximo-dorsal slope angle of the radial carpal bone (CrPDSA):** This was the angle formed
35 between the RL and the dorsal aspect of the proximal surface of Cr. A line representing the dorsal
36 slope of the proximal articular surface of Cr was drawn medially from the highest point of the
37 proximal articular surface of Cr through to its medial edge (Figure 5a: AB and Figure 5ai). If “line

1 AB” was drawn long enough, it will eventually meet the continuation of the RL and form the
2 proximo-dorsal slope angle of Cr (Cr PDSA) denoted by “x°”. A second line was drawn
3 perpendicularly from the RL to meet “line AB” at about its starting point to form angle “y” and was
4 measured, added to 90° and then subtracted from 180° get “x” (Figures 3 and 5a: AB).

5 **v. Distal slope angle of the ulnar carpal bone (CuDSA):** This was the angle formed by a Cu distal
6 topographic line “GH” drawn laterally from the medial edge of Cu articulation with Ci through to the
7 lateral edge of Cu (Figure 5a: GH) and “extended” to meet the RL. It was similarly represented as “x”
8 and calculated from $[x = 180 - (90+y)]$ as previously described above.

9 **vi. Disto-dorsal wedge angle of the intermediate carpal bone (CiDDWA):** This was the angle
10 formed at the dorsal articular ridge between the medial and lateral distal articular facets of Ci. A line
11 “JK” was drawn laterally from the point of Ci articulation with Cr and the articular ridge between the
12 radial and intermediate facets of C3 to the dorsal meeting point of Ci, C3 and C4 (Figure 5b: point
13 “K”) where it met with a second line “KL”. The second line which represented the lateral articular
14 facets of Ci was drawn medially from Ci articulation point with Cu extending to the Ci inter-facet
15 articular ridge where it met with the first line to form CiDDWA (Figure 5b: JKL).

16 **vii. Disto-dorsal wedge angle of the fourth carpal bone (C4DDWA):** This was the angle formed at
17 the articular ridge between the dorsal and lateral distal articular facets of C4. It was formed by 2 lines
18 (Figure 5b and Figure 5bi: a' b' c'). The first line representing the dorsal articular facet of C4 (a' b'),
19 started from the distal meeting point of the images of C3 and C4 and extended to the articular ridge
20 between the dorsal and lateral articular facets of C4. The second line (b' c') extended from this ridge to
21 the lateral margin of the lateral articular facet of C4.

22 **viii. Disto-palmar wedge angle of the fourth carpal bone (C4DPWA):** This was the angle formed
23 at the articular ridge between the palmar and lateral distal articular facets of C4 (Figure 5b and Figure
24 5bii: a b c'). It was represented by a line starting from medial margin of the palmar articular facet of
25 C4 extending to the ridge (a b) and another line from the ridge extending to the lateral margin of the
26 lateral articular facet of C4 (b c').

27 **ix. Width ratio of distal radius to proximal metacarpus (WDR:WPM):** This was the ratio of the
28 width of the distal radius as measured from its most lateral to its most medial side (Figure 5c and
29 Figure 5ci: AB) to the width of the proximal metacarpal bones as measured from the most lateral side
30 of MC4 to the medial margin of MC2 (Figure 5c and Figure 5ci: CD).

31 **x. Width ratio of distal radius' medial articular condyle to lateral articular condyle**
32 **(DRW.MAC:LAC):** This was the ratio of the width of medial articular condyle of the distal radius as
33 measured from its medial margin to the inter-condylar ridge (Figure 5c and Figure 5cii: aH) to the
34 width of the lateral articular condyle as measured from the inter-condylar ridge to its lateral margin
35 Figure 5c and Figure 5cii: Hb).

36 **2.3. Validation of consistency of position of landmarks for radiographic carpal parameters**

1 After the initial set of radiographs were acquired, the limbs were then dissected to expose the carpal
2 bones on both the dorsal and palmar aspects of the carpus and then radiographed a second time. A
3 radiopaque material (flexible metal wire) was then cut and fixed with super glue to the anatomic
4 features used as landmarks to develop the parameters and the limbs radiographed the third time. All
5 the limbs were thus radiographed 3 times each at ZDP, ZLM and ZML views (i.e as intact limb before
6 dissection; immediately after dissection and lastly after fixing the markers). The outline of the dorsal
7 and palmar borders of each carpal bone was differentiated on the studied radiographs as explained in a
8 standard radiographic anatomy text (Butler *et al.*, 2008).

9 **2.4. Statistical analysis**

10 All data were presented as Mean \pm standard deviation (SD). One-way repeated measure ANOVA was
11 used to compare means of each parameter measured from the three categories of carpal radiographs
12 (i.e. from intact, dissected and metal marked). A paired Student t-test was used to compare the
13 measurements from ZLM and ZML radiographs. Inter and intra observer reliability tests of
14 measurements were analysed using paired t-test, intra class correlation coefficient (ICC) and Bland-
15 Altman plot to chart the strength of agreement between the 2 independent observers. A Bland-Altman
16 plot is charted based on calculated mean difference of 2 separate measurements for the same variables
17 and the upper and lower 95% limit of agreement. A 95% confidence interval was used and values
18 where $P < 0.05$ were considered significant. All statistical tests were performed with MS Excel 2016
19 and Version 23 of IBM SPSS statistics for Windows.

20 **3. RESULTS**

21 14 parameters were developed from investigating the radiographic anatomy of the equine carpus. Four
22 parameters were developed from the ZLM image (view) and 10 from the ZDP image (Table 1). No
23 significant differences ($p > 0.05$) were observed between measurements obtained on the lateromedial
24 (ZLM) and the mediolateral (ZML) images and between measurements of carpal parameters on
25 radiographs from intact, dissected and metal marked limbs (Table 2). The differences between the
26 repeated measurements of the two observers (Table 3) were not significantly different and the inter-
27 observer ICC were generally good ranging from 0.581 to 0.969 (Table 4) except for WDR:WPM
28 where the ICC was below 0.5 (0.443) and considered poor. A Bland-Altman plot showing the strength
29 of agreement between the 2 observers was presented for each parameter (Figure 6a-n).

30 **4. DISCUSSION**

31 The data sets presented in this study for the 14 developed carpal parameters were generally
32 well distributed except for CiPxTRA that was skewed to the left (Table 1). Graphically, the normality
33 of a distribution (data set) is expressed by the dome shaped bell and it should appear symmetric if it
34 looks the same to the left and to the right of the center point (Asghar & Zahediasl, 2012; Mishra et al.,
35 2019). Skewness is the measure of lack of symmetry (i.e. asymmetry) of a normal distribution (data
36 set). Ideally, for a symmetric distribution, the mean, median, and mode would coincide, and its
37 skewness statistic = 0, but that hardly happens in most data set. Thus, distributions are considered

1 “approximate normal” if value is between -1 and $+1$ and considered highly skewed when less than -1
2 or greater than $+1$ (Asghar & Zahediasl, 2012; Mishra et al., 2019). A stricter value of between -0.5
3 and 0.5 for approximately symmetric, and between -1 and -0.5 or between 0.5 and 1 for moderately
4 skewed is sometimes used for interpretation. It is difficult at this stage to ascertain the source or
5 reason for the negative skewness of CiPxTRA observed in this study as it could either be a sample
6 skewness without skewness in the population or an indication of skewness in the population.

7 The metal markers used in this study, made the landmarks used for the development of the
8 parameters to be more visible (radiopaque) and thus reduced the chance of missing these points of
9 interest. Measurements that were acquired with the aid of markers affixed to landmarks could
10 therefore be regarded as true and accurate representations of distances or angles between two or
11 more points of interest. Since there were no significant differences between measurements of the same
12 parameters evaluated on radiographs from the marked and non marked preparations of same limb, it is
13 reasonable to suggest that the measurements acquired without markers were as reliable as those with
14 markers. This therefore validates that the location of the landmarks used on the radiographs were
15 consistent and repeatable. The necessity for verification of new methods suggests that measurement
16 be taken more than once and also by more than one observer for comparison. Analysis of these
17 repeated measures validate the consistency and repeatability of the method of measurement and the
18 parameters been measured. The high intraclass correlation coefficient (ICC), found between and
19 within measurements of the 2 observers in this study, thus further suggest clarity of parameters’
20 landmarks and the ease and simplicity of the methodology.

21 Bland-Altman plot was introduced by Altman and Bland (1983) to describe the
22 correlation or agreement more accurately between 2 quantitative measurements. It constructs on a
23 scatter plot XY, the calculated mean difference (bias), and an upper and lower limit of agreement
24 (LOA) between these 2 measurements. The Y axis shows the difference between the 2 paired
25 measurements while the X axis represent the average of the 2 measurements (Giavarina, 2015). 95%
26 of the data points are expected to be within ± 2 standard deviation of the mean difference (centered
27 line), represented by the 2 straight lines of upper and lower LOA respectively (Altman & Bland,
28 1983; Giavarina, 2015; Dogan, 2018). A strong inter-rater agreement observed in this study for all the
29 14 parameters could further affirm the accuracy, reliability, and reproducibility of measurements.
30 Radiographic parameters were developed with the intent of measuring different aspects of the
31 conformation of the equine carpus, so that when one or more parameters are evaluated together, a
32 more comprehensive assessment of the carpus can be achieved.

33 The dorsal carpal angle (DCA) was developed to measure the general alignment of the carpus
34 as viewed from the lateral aspect of the forelimb of the horse. Although the method used to measure
35 DCA in this study was based primarily on the procedure described by Barr (1994), the term DCA was
36 however not used in Barr’s report. Other authors (Burn *et al.*, 2006; Deane & Davies, 1995b) have
37 differently measured “carpal angle” also from the lateromedial view while still using the intersection

1 of the long axis of the antebrachium and the third metacarpal bone. They referred to the angle formed
2 at the palmar aspect of the carpus as the “carpal angle”. Confusion could therefore arise as to what
3 orientation best defined the carpal angle or its proper nomenclature. The term DCA was therefore
4 adopted in the current study to precisely identify the anatomical plane for which the angle has been
5 measured. The term “hyperextension” is often used to describe overextending of a joint and carpal
6 hyperextension has been reported to be associated with carpal damages and conformational
7 unsoundness of the carpus in horses (Fretz, 1980; Barr, 1994; Deane & Davies, 1995b; Kainer, 2002;
8 Stashak & Hill, 2002; Burn *et al.*, 2006). DCA measures the degree to which a carpus is either
9 conformationally hyperextended (back-at-the-knee) or flexed (“Buck-kneed”). Also, during exercise,
10 DCA could be used to either experimentally (Olusa *et al.*, 2019) or physiologically (Burn *et al.*, 2006;
11 Deane & Davies, 1995b) assess the severity (degree) of hyperextension of the carpus at loading phase
12 of locomotion.

13 The third carpal bone palmar facet angle (C3PalFCA) was conceived to measure the
14 alignment of the middle carpal joint. Since the C3 palmar facet is a feature within the middle carpal
15 joint, it was thought that the angle formed by its relative height with the dorsal margin of the proximal
16 row of carpal bones, might affect either the forward or backward tilt of the proximal row of carpal
17 bones, the distal antebrachium during loading and subsequently the entire carpal conformation. The
18 middle carpal joint is a frequently damaged joint therefore, any parameter that can be used to assess
19 its alignment (hyperextension) might be useful in diagnosis of middle carpal joint injuries and
20 understanding of their pathogenesis. In a recent study, C3PalFCA was found useful for assessing the
21 degree (severity) of carpal hyperextension as its values increase with increasing loading of the carpus
22 (Olusa *et al.*, 2019). It also gave a more holistic evaluation of the carpus when assessed along with
23 DCA as it was found to be inversely related to DCA (Olusa *et al.*, 2019).

24 The distal radial slope carpal angle (DRSCA) was designed to measure the conformational
25 alignment of the disto-dorsal portion of the antebrachium (epiphysis) with the proximal row of carpal
26 bones while the intermediate carpal bone proximal tuberosity-radial angle (CiPxTRA) attempts to
27 assess the angular alignment formed between the highest point of the proximal row of carpal bones
28 (the palmar tuberosity of Ci) and the disto-dorsal rim and epiphyseal slope of the radius. The palmar
29 tuberosity of Ci has been reported to be more developed in the thoroughbred than in the pony
30 (Abdunnabi *et al.*, 2011). CiPxTRA might therefore be helpful in further assessment of the degree of
31 carpal hyperextension as it relates to or originates from the antebrachiocarpal joint.

32 The term “medial carpal angle” (MCA) has not been previously used to describe the
33 measurement of “carpal angle” from the frontal plane of live horses, or on photographs of horses and
34 on DPa radiographs. Nevertheless, the use of the intersection or pivot point of the radius and the third
35 metacarpal bone has long been used in the horse especially when assessing the severity of angular
36 limb deformities in foals (Butler, 2008; Fretz, 1980; Steinman *et al.*, 2000). MCA purpose was to
37 measure the general alignment of the forelimb at the level of the carpus as viewed in the frontal plane.

1 This can be used routinely/clinically to objectively quantify the degree of carpal valgus or varus in the
2 horse instead of the subjective method of dropping an imaginary line from the point of the shoulder
3 joint to bisect the limb (Stashak & Hill, 2002). It will also be useful in assessing the degree of
4 extension or hyperextension during loading and flexion of the carpus (Olusa *et al.*, 2019).

5 The current study measured for the first time the wedge-like angulations of the articular
6 surfaces of the equine carpal bones. Although the interlocking wedge concept of the carpal bones
7 have been described (Bramlage, 1988; Deane & Davies, 1995a; Rooney, 1969; Von Rubeli, 1925)
8 there are no published measurements of these angles. Quantifying the topographic geometry of each
9 carpal bone articular surfaces (Sledge, 1993), may however open a new area of investigation into how
10 the biomechanics of the smooth load transmission from bone to ligament has protected the carpus
11 from injury during the evolution of the horse.

12 The C3DDSA measures the angulation of the distal articular surface of C3. Since C3 is
13 subjected to high compressional forces during loading (Bramlage, 1988; Palmer, 1994; Young *et al.*,
14 1991), the steepness of this angle might have a possible correlation with how the C3 is
15 conformationally stable on the MC3 during loading. In a study carried out by Abdunnabi (2011), out
16 of 5 parameters that were used to categorize two limbs into “favourable” or “less favourable” carpal
17 conformation and used to assess their stability under loading, 3 were related to the C3 (Abdunnabi,
18 2011). Other parameters related to C3 that were developed in the current study were CrDDSA and
19 CiDDWA. The CrDDSA measures the steepness of the radial articular facet of C3 while CiDDWA
20 partly measures the steepness of the intermediate articular facet of C3. The clinical extent of congruity
21 maintained by Cr and Ci on C3 and on the proximal metacarpus by C3 during loading would be based
22 on the degree of steepness and wedgeness of their articular surfaces and facets. Measuring the shape
23 and geometrical properties of C3 might therefore provide a useful tool for quantifying the
24 contributory role of C3 to the stability of the carpal joint in horses.

25 The wedge-like angulations of the distal surface of C4 promote its stability in-between the
26 lateral splint bone, the third metacarpal bone and the C3 during loading. The steepness of these
27 wedge-like angles of C3 and C4 could have important roles in the conformational stability of the
28 distal carpal row which would be essential to the integrity of the carpometacarpal joint. On its
29 proximal articular surface, the C4 articulates with the distal articular surface of ulnar carpal bone (Cu)
30 during loading and thus CuDSA attempts to estimates the degree of congruity between the opposing
31 surfaces of Cu and C4 under load.

32 The unique morphology of Ci has positioned it as the prime example of the wedge concept
33 (Bramlage, 1988; Deane & Davies, 1995a; Rooney, 1969) and a clear depiction of the wedge-like
34 angulation of the articular surfaces of the carpal bones (Bramlage, 1988). CiDDWA was conceived to
35 measure the conformational stability of the Ci as it stabilizes/wedges between the C3 and C4 during
36 weight bearing. The presence and degree of this angle might have an important role in the transfer of
37 axial forces to the intercarpal ligaments between these bones. Auer *et al.*, (1986) suggested that

1 spinning (rotational) movements occur around the long axes of the antebrachium and MC3 as the
2 carpus is moving into a close-packed position during loading and that fractures of C4 and Ci are due
3 to abnormal concentration of forces on these 2 bones. If the radius is rotating outward from medial to
4 lateral (supination), while the MC3 is stationary or rotating lateromedially (i.e. inwardly and termed
5 pronation), C4 and Ci are believed to be slammed together before other carpal bones can make full
6 contact (Auer *et al.*, 1986). A steeper CiDDWA might therefore increase the slamming rate and
7 impact of collision between these bones and result in increased incidence and severity of damage.
8 Being able to measure this angle and ultimately establishing a safe value range for conformationally
9 stable Ci may further help our understanding of loading, load transfer to adjacent bones and ligaments
10 and pathogenesis of middle carpal joint damage.

11 Both the proximal and distal articular surface slope angles of Cr were measured. These
12 measurements assess the degree of congruity of the proximal surface of the Cr with the radius and the
13 distal surface of the Cr with the C3. The Cr is perhaps the most mobile of the carpal bones and
14 receives high loading stress during flexion and extension of the antebrachiocarpal and middle carpal
15 joints. A suggested mechanism of injury to these joints was repeated carpal hyperextension and
16 resultant shortening (weakening) or microanatomic fractures of articular surfaces due to the chronic
17 accumulation of loading stress (Bramlage, 1988). A deformed (weakened) articular surface may
18 perhaps be measurable by assessing changes in the wedge angles. Furthermore, an increase or
19 decrease in the steepness of these angles (CrDDSA and CrPDSA) might affect the loading stability of
20 the Cr as it wedges in between the radius and the C3.

21 The width of the distal antebrachium would represent the proximal boundary of the carpus
22 while the width of the metacarpus would represent the distal perimeter of the carpus. These 2
23 boundaries were measured as a ratio of each other (WDR:WPM). If a large difference exists between
24 these 2 surfaces/width, it might result in a “funnel effect” in which a load travelling from the
25 antebrachium will exert more pressure (strain) on the metacarpus due to the smaller recipient contact
26 area. More studies will be required to test this theory.

27 DRW.MAC:LAC measures the relative width of the distal radius condyles. In another study,
28 a similar measurement of widths of the lateral and the medial condyles of the distal extremity of MC3
29 showed that the medial condyle width was significantly larger than the lateral condyle (Alrtib *et al.*,
30 2012). This was thought to partly prevent the sliding of the proximal phalanx towards the lateral
31 direction; a reason believed to be associated with the low incidence of fetlock luxation in horses
32 (Alrtib *et al.*, 2012; Bertone, 2002). In the present study, the width of the medial articular condyle
33 (MAC) of the distal radius was consistently less than the width of the lateral articular condyle (LAC).
34 This would contribute to the conformational stability of the radius on the proximal carpal row as well
35 as the general carpal alignment.

36 5. CONCLUSION

1 This study developed a radiographic measurement protocol and proposed 14 parameters for
2 objective assessment of carpal conformation in the horse. These parameters are more holistic and yet
3 simple to measure in comparison to previous methods. 5 of these 14 parameters were already found
4 useful/relevant for assessing carpal conformation during experimental loading and flexion of the
5 carpus (Olusa *et al.*, 2019). This evaluation protocol can be easily incorporated into routine
6 radiographic examination of the horse such as pre purchase examination. With further studies on
7 larger equine populations, and establishment of ranges of normal values for these parameters in
8 different breeds, this technique offers a potential tool for clinicians for assessing different angular
9 limb (carpal) conformation and physiological hyperextension in horses. This approach when adopted
10 could also help to eliminate the often-encountered judgemental errors or variation between equine
11 practitioners using subjective visual assessment for the carpus. Further investigation will be required
12 for comparison between subjective visual examination and objective radiographic assessment
13 methods of carpal conformation.

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20 **CONFLICT OF INTEREST**

21 No conflict of interest is declared for this work.

23 **DATA AVAILABILITY STATEMENT**

25 The data that support the findings of this study are available from the corresponding author upon
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Table 1: 14 Carpal conformational parameters measured from Zero lateromedial (ZLM) and Zero dorsopalmar (ZDP) radiographs of 10 cadaveric limbs

S/no	Measurable Parameters (n=10)	Mean ± SD (°)	Median (°)	95% C I of Mean		Skewness Statistic
				Lower	Upper	
1	DCA	176.61±0.66	176.79	176.14	177.08	-0.529
2	DRSCA	145.59±2.19	145.65	144.02	147.15	0.607
3	CiPxTRA	115.69±3.15	117.24	113.44	117.94	-1.495**
4	C3PalFCA	84.43±1.13	84.48	83.62	85.24	-0.502
5	MCA	183.34±1.02	183.49	182.61	184.07	-0.314
6	C3DDSA	8.27±0.92	8.21	7.61	8.93	0.638
7	C4DDWA	141.71±2.85	140.71	139.67	143.75	0.657
8	C4DPWA	128.31±5.03	129.67	124.72	131.91	-0.219
9	CrDDSA	7.91±1.16	8.07	7.08	8.74	0.249
10	CrPDSA	13.44±0.87	13.48	12.81	14.06	-0.077
11	CiDDWA	153.08±2.19	153.39	151.52	154.64	-0.368
12	CuDSA	33.02±2.77	32.44	31.04	35.01	0.649
13	WDR: WPM	1.13±.03	1.13	1.11	1.15	0.583
14	DRW.MAC:LAC	0.77±0.06	0.79	0.72	0.81	-0.244

DCA = Dorsal carpal angle; DRSCA = Distal radial slope carpal angle; CiPxTRA = Intermediate carpal bone proximal tuberosity-radial angle; C3PalFCA = third carpal bone palmer facet angle; MCA = Medial carpal angle; C3DDSA = Disto-dorsal slope angle of the third carpal bone; C4DDWA = Disto-dorsal wedge angle of the fourth carpal bone; C4DPWA = Disto-palmar wedge angle of the fourth carpal bone; CrDDSA = Disto-dorsal slope angle of the radial carpal bone; CrPDSA = Proximo-dorsal slope angle of the radial carpal bone; CiDDWA = Disto-dorsal wedge angle of the intermediate carpal bone; CuDSA = Distal slope angle of the ulnar carpal bone; WDR:WPM = Width ratio of distal radius to proximal metacarpus; DRW.MAC:LAC = Width ratio of distal radius' medial articular condyle to lateral articular condyle. 95% C I = 95% Confidence interval; (°) = Degrees. The unit of measurement was in degree for all the parameters except for WDR:WPM and DRW.MAC:LAC that are ratios and had no unit. SD = Standard deviation. btw = between. ** = highly skewed

Skewness statistic measures lack of symmetry (asymmetry) of normal distribution of a data set. perfect symmetric = 0; approximate normal/symmetric = btw -0.5 and 0.5; moderately skewed = btw -1 and -0.5 or 0.5 and 1; and highly skewed = less than -1 or greater than 1.

Table 2: Validation of the consistency of the positions of landmarks used for measuring the 14 carpal parameters from ZLM and ZDP radiographs

S/no	Measurable Parameters (n = 10)		Mean ± SD (°)					Sig. btw int, dis & mak carpi (p<0.05)*	
			Intact limb/ Carpi	Sig. (p value) btw ZLM & ZML	Dissected limb/ Carpi	Sig. (p value) btw ZLM & ZML	Carpi with marker		Sig. (p value) btw ZLM & ZML
1	DCA	ZLM	176.61±0.66	0.273	176.45±0.81	0.265	176.88±0.62	0.286	0.403
		ZML	176.25±0.50		176.79±0.48		176.46±0.77		
2	DRSCA	ZLM	145.59±2.19	0.789	144.89±1.73	0.643	145.22±1.81	0.828	0.725
		ZML	145.87±2.09		144.61±1.69		145.07±1.68		
3	CIPxTRA	ZLM	115.69±3.15	0.981	114.82±1.91	0.582	115.93±2.49	0.850	0.602
		ZML	115.72±2.01		115.47±2.33		115.79±1.95		
4	C3PalFCA	ZLM	84.43±1.13	0.574	84.71±1.95	0.924	85.26±2.03	0.709	0.567

		ZML	84.81±1.66		84.78±1.85		84.95±1.58		
5		MCA	183.34±1.02	na	183.99±1.33	na	183.89±1.36	na	0.463
6		C3DDSA	8.27±0.92	na	8.02±0.81	na	8.08±0.90	na	0.807
7		C4DDWA	141.71±2.85	na	141.24±3.00	na	142.17±3.21	na	0.791
8		C4DPWA	128.31±5.03	na	128.18±4.09	na	128.22±5.68	na	0.998
9		CrDDSA	7.91±1.16	na	7.64±0.88	na	8.16±1.01	na	0.536
10		CrPDSA	13.44±0.87	na	13.45±1.36	na	13.52±1.82	na	0.990
11		CiDDWA	153.08±2.19	na	151.62±2.76	na	153.63±3.11	na	0.250
12		CuDSA	33.02±2.77	na	33.19±3.00	na	35.05±3.27	na	0.269
13		WDR:WPM	1.13±0.03	na	1.13±0.02	na	1.13±0.03	na	0.821
14		DRW.MAC:LAC	0.77±0.06	na	0.78±0.04	na	0.77±0.06	na	0.828

DCA = Dorsal Carpal Angle; DRSCA = Distal Radial Slope Carpal angle; CiPxTRA = Intermediate carpal bone Proximal Tuberosity-Radial Angle; C3PalFCA = Third carpal bone Palmer facet angle; MCA = Medial Carpal angle; C3DDSA = Disto-dorsal slope angle of the third carpal bone; C4DDWA = Disto-dorsal wedge angle of the fourth carpal bone; C4DPWA = Disto-palmar wedge angle of the fourth carpal bone; CrDDSA = Disto-dorsal slope angle of the radial carpal bone; CrPDSA = Proximo-dorsal slope angle of the radial carpal bone; CiDDWA = Disto-dorsal wedge angle of the intermediate carpal bone; CuDSA = Distal slope angle of the ulnar carpal bone; WDR:WPM = Width ratio of Distal radius to Proximal metacarpus; DRW.MAC:LAC = Width ratio of distal radius' medial articular condyle to lateral articular condyle. 95% CI = 95% Confidence interval; SD = Standard deviation; na = non applicable; btw = between; * = Statistical significance (Sig.) at p<0.05. int = intact, dis = dissected, mak = marked.

Table 3: Intra-observer repeatability (test re-test reliability) test for each of the 14 carpal parameters measured separately by 2 independent observers.

Results showed no significant mean difference and intraclass correlation coefficient (ICC) between their (i.e. Obr 1 & 2) respective 2 repeated measurements.

S/ no	Parameters (n = 10)	Mst/ Reading	Observer 1				Observer 2			
			Mean±SD	Mean Diff.±SD	Sig. (p<0.05)*	ICC (95% CI)	Mean±SD	Mean Diff.±SD	Sig. (p<0.05)*	ICC (95% CI)
1	DCA	1 st	176.61±0.66	0.20±0.64	0.344	0.616	176.52±0.60	-0.02±0.69	0.925	0.660

		2 nd	176.41±0.56			(-0.464; 0.903)	176.54±0.72			(-0.542; 0.918)
2	DRSCA	1 st	145.59±2.19	0.16±1.55	0.755	0.808 (0.188; 0.953)	145.98±1.33	0.67±1.62	0.494	0.668
		2 nd	145.43±1.47				145.31±1.85			(-0.356; 0.918)
3	CiPxTRA	1 st	115.69±3.15	0.07±0.92	0.811	0.975 (0.899; 0.994)	116.55±1.29	0.32±0.81	0.244	0.895
		2 nd	115.62±2.46				116.24±1.39			(0.607; 0.974)
4	C3PalFCA	1 st	84.43±1.13	0.09±1.09	0.785	0.744 (-0.108; 0.938)	84.57±1.85	-0.18±1.78	0.759	0.620
		2 nd	84.33±1.22				84.75±1.46			(-0.709; 0.908)
5	MCA	1 st	183.34±1.02	-0.04±0.78	0.881	0.852 (0.379; 0.964)	183.61±1.05	-0.42±0.73	0.867	0.753
		2 nd	183.38±1.08				184.03±0.94			(-2.799; 0.795)
6	C3DDSA	1 st	8.27±0.92	-0.26±0.31	0.027	0.949 (0.670; 0.989)	8.29±0.58	-0.09±0.55	0.624	0.852
		2 nd	8.52±0.80				8.38±0.88			(0.401; 0.963)
7	C4DDWA	1 st	141.71±2.85	-0.39±1.08	0.280	0.951 (0.813; 0.988)	142.41±2.39	-0.06±1.94	0.924	0.806
		2 nd	142.10±2.15				142.47±2.26			(0.166; 0.953)
8	C4DPWA	1 st	128.31±5.03	-0.37±1.02	0.273	0.989 (0.960; 0.997)	128.83±6.01	0.10±2.01	0.874	0.965
		2 nd	128.69±5.09				128.73±4.22			(0.856; 0.991)
9	CrDDSA	1 st	7.91±1.16	-0.01±0.38	0.909	0.973 (0.891; 0.993)	8.14±0.77	-0.08±0.59	0.664	0.846
		2 nd	7.93±1.05				8.22±0.80			(0.370; 0.962)
10	CrPDSA	1 st	13.44±0.87	-0.15±0.91	0.606	0.845 (0.372; 0.962)	13.23±1.25	-0.05±0.65	0.810	0.924
		2 nd	13.59±1.48				13.28±1.09			(0.688; 0.981)
11	CiDDWA	1 st	153.08±2.19	0.27±0.91	0.379	0.957 (0.838; 0.989)	153.24±1.96	0.44±0.73	0.093	0.963
		2 nd	152.81±2.29				152.80±2.35			(0.836; 0.991)
12	CuDSA	1 st	33.02±2.77	0.36±0.63	0.099	0.985 (0.931; 0.996)	32.62±2.63	0.18±0.71	0.447	0.982
		2 nd	32.66±2.86				32.44±2.56			(0.930; 0.995)
13	WDR:WPM	1 st	1.13±0.03	-0.001±0.02	0.876	0.852 (0.377; 0.964)	1.13±0.03	0.001±0.02	0.859	0.883
		2 nd	1.13±0.02				1.13±0.02			(0.512; 0.971)

14	DRW.MAC:	1 st	0.77±0.06	-0.008±0.04	0.534	0.866 (0.467; 0.966)	0.78±0.05	0.01±0.06	0.761	0.802 (0.404; 0.885)
	LAC	2 nd	0.77±0.05				0.77±0.05			

Measurement (Mst) Reading refers to the separate 1st and 2nd time points (minimum of 2 weeks interval) of repeated measurement of radiographs by the two observers. **95%**

CI = 95% Confidence interval. **Mean Diff** = Difference between 2 means. **SD** = Standard deviation. * = Statistical significance (**Sig.**) at **p<0.05**

Table 4: Assessment of agreement of measurement between the 2 independent observers (Inter-rater reliability test) for each of the 14 carpal parameters using calculated mean difference (bias) and 95% limit of agreement (CI) for the Bland-Altman plot

S/ no	Parameters	Observers	Mean±SD	Mean Diff.±SD	Sig (p<0.05)*	Intraclass Correlation Coefficient (95% CI)	Calc. 95% CI for Limits of agreement (for Bland-Altman plot)	
							Lower	Upper
1	DCA	1 st	176.61±0.66	0.09±0.83	0.739	0.621 (-1.855; 0.922)	-1.5324	1.7124
		2 nd	176.52±0.60					
2	DRSCA	1 st	145.59±2.19	-0.39±0.97	0.844	0.823 (0.248; 0.957)	-2.3002	1.5142
		2 nd	145.98±1.33					
3	CiPxTRA	1 st	115.69±3.15	-0.86±2.81	0.257	0.884 (0.165; 0.987)	-6.3694	4.6454
		2 nd	116.55±1.29					
4	C3PalFCA	1 st	84.43±1.13	-0.14±2.03	0.735	0.732 (-0.174; 0.820)	-4.1168	3.8408
		2 nd	84.57±1.45					
5	MCA	1 st	183.34±1.02	-0.27±1.71	0.096	0.581 (-0.547; 0.834)	-3.6309	3.0829
		2 nd	183.61±1.54					
6	C3DDSA	1 st	8.27±0.92	-0.02±0.59	0.914	0.907 (0.307; 0.987)	-1.1939	1.1519
		2 nd	8.29±0.58					
7	C4DDWA	1 st	141.71±2.85	-0.70±1.52	0.177	0.922 (0.539; 0.989)	-3.6849	2.2769
		2 nd	142.41±2.39					

8	C4DPWA	1 st	128.31±5.03	-0.52±1.27	0.228	0.989 (0.895; 0.998)	-3.0054	1.9674
		2 nd	128.83±6.01					
9	CrDDSA	1 st	7.91±1.16	-0.22±0.55	0.228	0.916 (0.564; 0.987)	-1.3473	0.8993
		2 nd	8.14±0.77					
10	CrPDSA	1 st	13.44±0.87	0.20±0.99	0.532	0.789 (-0.269; 0.970)	-1.7406	2.1486
		2 nd	13.23±1.25					
11	CiDDWA	1 st	153.08±2.19	-0.16±1.42	0.731	0.969 (0.769; 0.995)	-2.9519	2.6319
		2 nd	153.24±1.96					
12	CuDSA	1 st	33.02±2.77	0.41±1.38	0.373	0.872 (0.861; 0.927)	-2.2888	3.1048
		2 nd	32.62±2.63					
13	WDR:WPM	1 st	1.13±0.03	-0.01±0.03	0.614	0.443 (-2.686; 0.883)	-0.0643	0.0543
		2 nd	1.13±0.03					
14	DRW:MAC:LAC	1 st	0.77±0.06	-0.01±0.05	0.521	0.869 (0.542; 0.989)	-0.1029	0.0829
		2 nd	0.78±0.05					

Estimates of reliability based on ICC values are categorized as follows: below 0.5 = Poor; 0.5 to 0.75 = Moderate; 0.75 to 0.9 = Good and above 0.9 = Excellent (Koo & Li 2016). * = Statistical significance (**Sig.**) at **p<0.05**

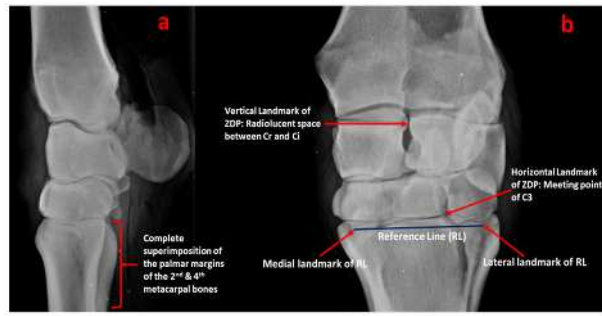
Table 5: (Appendix) Abbreviations and details of technical parameters used for imaging

DP	Dorsopalmar: This refers to the direction of travel of the primary X-ray beam as viewed from the frontal plane of the horse/limb. The beam enters on the dorsal surface of the carpus and exit from the palmar side
LM	Lateromedial: This refers to the direction of travel of the primary X-ray beam as it enters on the lateral side of the limb and exit from the medial side

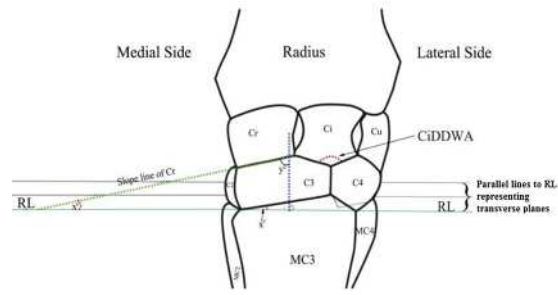
ML	Mediolateral: X-ray beam travelled in opposite direction to LM
ZDP	Zero dorsopalmar: This is an oblique variation of dorsopalmar view. It is usually obtained when the direction of travel of the primary X-ray beam entered the object at between 2° to 15° Dorsolateral-Palmaromedial Oblique (DL-PaMO). The angulation of the oblique depends on the conformation of each limb. The aim was to produce a radiograph of the carpus with i) a small radiolucent space between the proximo-dorsal articular facets of the radial carpal bone (Cr) and intermediate carpal bone (Ci); and ii) a contact point between the disto-lateral ends of the dorsal and the palmar borders of the third carpal bone (C3). These 2 features respectively served as the vertical and horizontal landmarks for ZDP view
ZLM	Zero Lateromedial: This was essentially a Palmarolateral-Dorsomedial Oblique (PaL-DMO) view. The oblique angle varied from between 5° to 20° depending on each limb's conformation. The aim of this view was to produce a radiograph in which the overlapped 4 th and 2 nd metacarpal bones were completely superimposed; represented by a single clear margin of their palmar borders
ZML	Zero Mediolateral: This was opposite to ZLM as the direction of travel of the primary X-ray beam was Dorsomedial-Palmarolateral Oblique (DM-PaLO) at similar angles
DICOM	Digital imaging and communication in medicine
PACS	Picture archiving and communication system



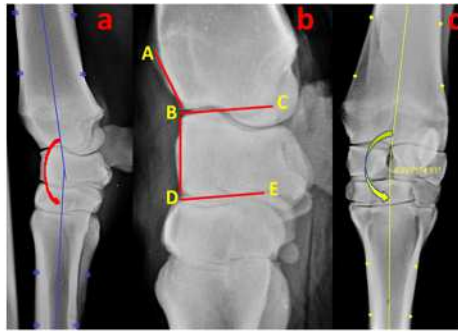
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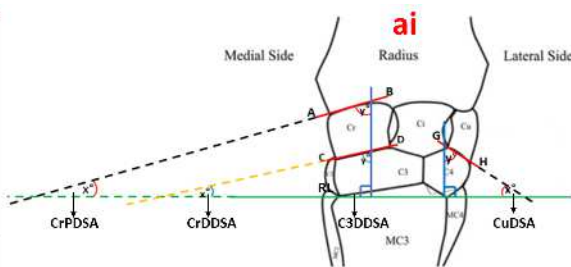
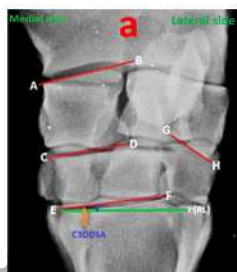
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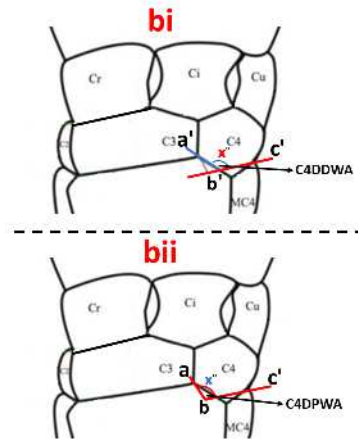
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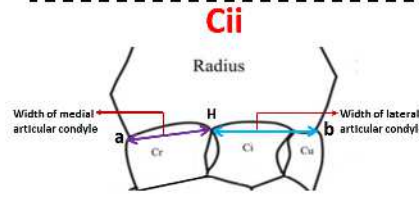
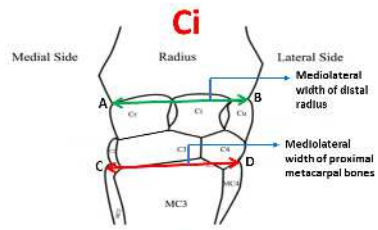
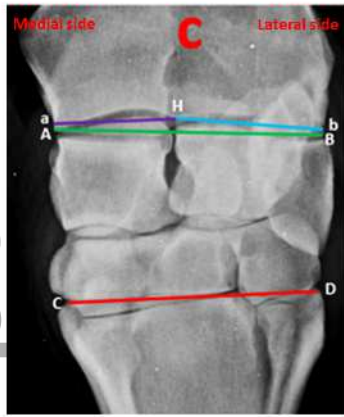
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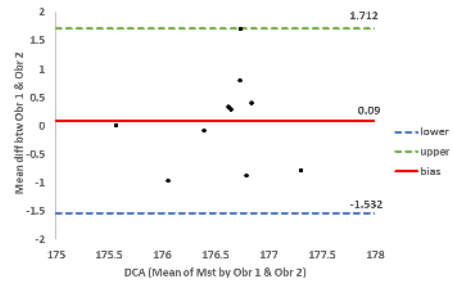
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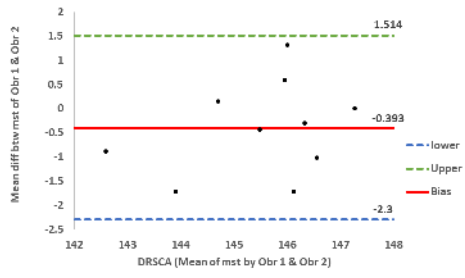
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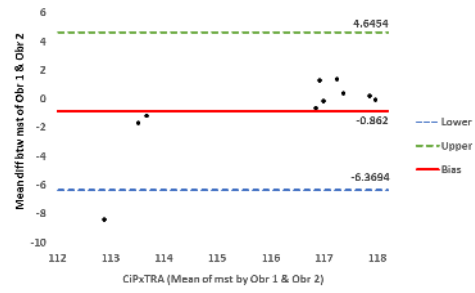
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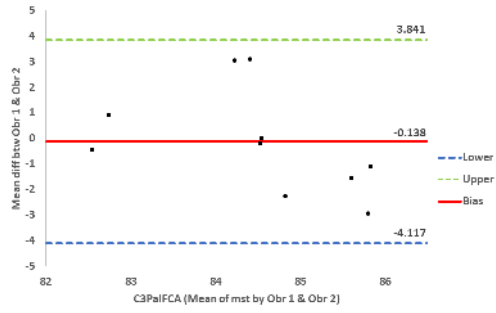
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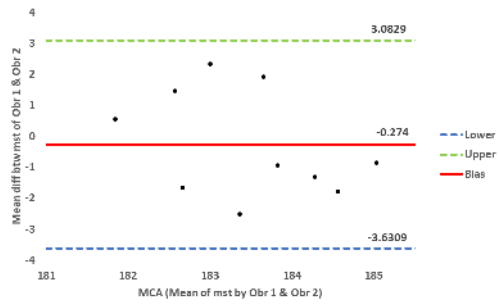
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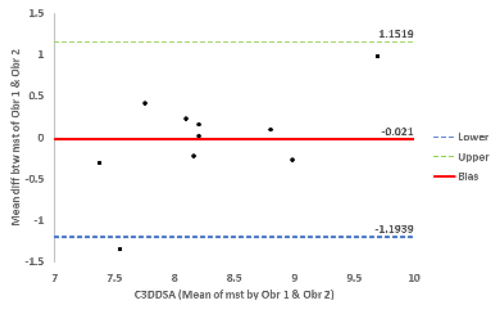
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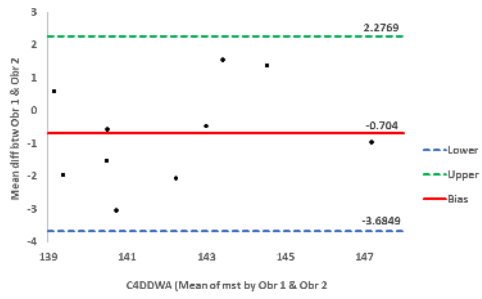
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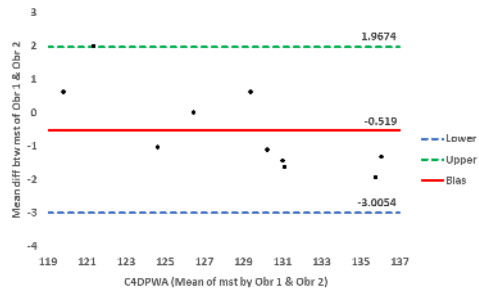
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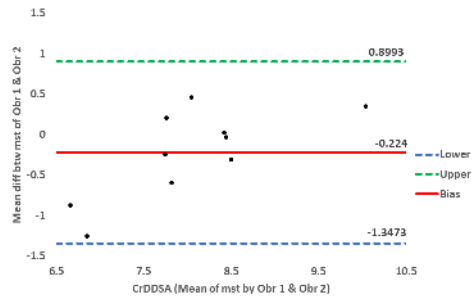
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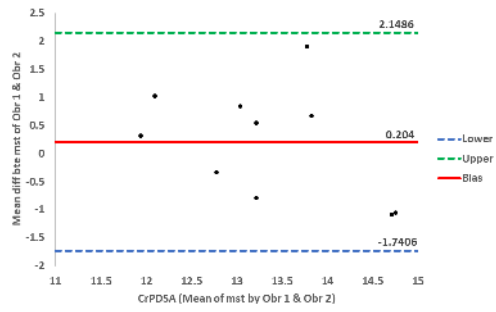
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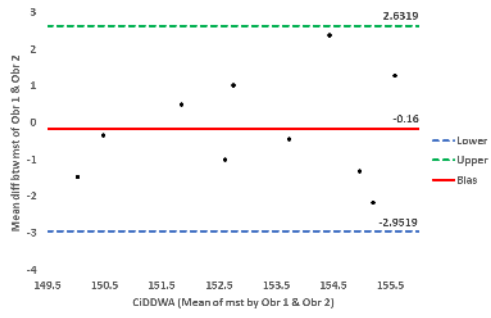
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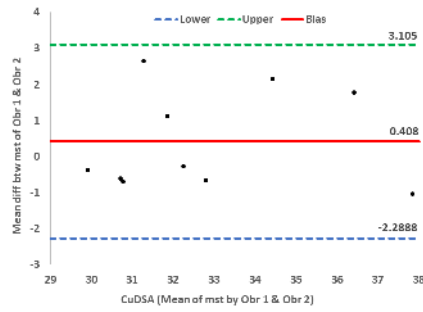
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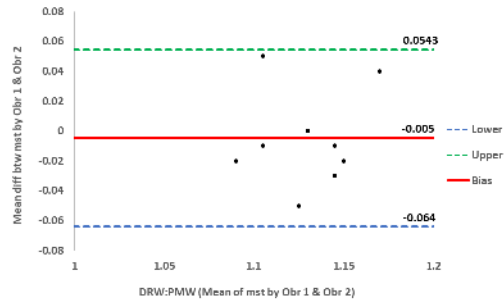
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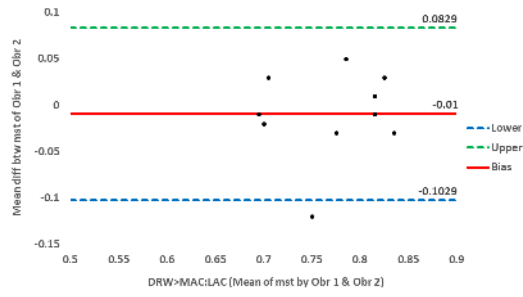
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