

1 EFFECTS OF IMAGE PLANE, PATIENT POSITIONING, AND FORAMINAL ZONE ON MAGNETIC  
2 RESONANCE IMAGING MEASUREMENTS OF CANINE LUMBOSACRAL INTERVERTEBRAL  
3 FORAMINA

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16  
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19  
20 Running Head: LS foramina dimension in 2 planes and 2 positions

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34 Abstract

35 Degenerative lumbosacral stenosis has been suspected to have a dynamic component, especially  
36 regarding encroachment of the L7 nerve roots exiting the lumbosacral foramina. Angled cross-  
37 sectional imaging of the neuroforamina has been found improve the accuracy of the diagnosis of  
38 stenosis in humans. In this anatomic study, foraminal apertures were evaluated by magnetic  
39 resonance imaging (MRI) at the entry, middle and exit zones of the nerve roots in 30 dogs that  
40 were clinically affected by lumbosacral disease. Standard versus oblique planar orientation and  
41 neutral versus hyperextended positioning of the lumbosacral area were compared by  
42 measuring the median values for entry, middle and exit zones. The neuroforaminal area  
43 acquired using oblique plane acquisition was significantly smaller than standard parasagittal  
44 measurements. Furthermore, standard parasagittal neuroforaminal dimensions in the

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45 hyperextended position were significantly smaller than standard parasagittal measurements in  
46 the neutral position. This statistical difference was even more pronounced for neuroforaminal  
47 dimension evaluated in the oblique plane and hyperextended position. Positioning of the dog  
48 during imaging has a significant effect on neuroforaminal dimension, corroborating the notion  
49 that spinal position may influence neural claudication in clinically affected patients. Reductions  
50 in neuroforaminal dimension are more evident on oblique planar image acquisition, suggesting  
51 that this approach may be more useful than parasagittal imaging as a tool for identifying subtle  
52 changes in L7 neuroforaminal dimensions in cases of canine lumbosacral stenosis.

53

## 54 Introduction

55 Lumbosacral disease in dogs is characterized by pain, lameness, reluctance to exercise and in  
56 case of compression of the cauda equina or L7 nerve roots exiting the lumbosacral foramina, by  
57 neurological impairment.<sup>1</sup> One major cause of lumbosacral disease or cauda equina syndrome is  
58 degenerative lumbosacral stenosis (DLSS).<sup>2,3</sup> Clinical symptoms of dogs suffering from  
59 lumbosacral stenosis can be exacerbated by exercise and certain movements,<sup>4-8</sup> and it is often  
60 seen in working dogs and dogs with high activity levels.<sup>9</sup> It is well accepted in humans that  
61 neuroforaminal impingement may be exacerbated by certain postural orientations and by axial  
62 loading of the spine.<sup>10</sup> In people it has been shown that walking and being in an upright position  
63 (extension of the spine and axial loading) make the symptoms worse.<sup>11</sup> The canine lumbosacral  
64 spine has been evaluated with flexion-extension myelography<sup>12</sup> and radiographic stress views.<sup>13</sup>  
65 In these studies it was stated that overextension of the spine was necessary to establish a  
66 diagnosis via myelography<sup>12</sup> and that static and dynamic components are involved in the  
67 compression and both should be evaluated.<sup>13</sup> Thereby it is proposed that lumbosacral stenosis  
68 and neurogenic claudication is a dynamic phenomenon and that the patient population would  
69 profit from being able to evaluate intervertebral foramina dimensions under dynamic  
70 conditions using an imaging procedure that makes measurements of the foraminae the most  
71 accurate.

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72 Cadaveric studies in humans have shown that flexion increased the size of the foraminal area by  
73 12% and extension decreased the area by 15%; with a 15.4% incidence of nerve root  
74 compression in the flexion group and 33.3% in the extension group.<sup>14</sup> Conventional recumbant  
75 MRI has been found to be inadequate for complete and thorough evaluation of the spinal column  
76 and its contents in humans.<sup>15</sup> Positional MRI demonstrated that minor neural compromise and  
77 positional pain score differences were significantly related to changes in foraminal size,<sup>11</sup> when  
78 MRI is performed in supine, erect-flexed and erect-extended positions.<sup>16</sup> Positional computed  
79 tomography (CT) has been found to be a feasible technique for quantifying dynamic changes in  
80 L7-S1 intervertebral foraminal morphology in dogs with lumbosacral disease<sup>17</sup> but a large  
81 variability in lumbosacral intervertebral foramen cross-sectional areas with a large  
82 interobserver variability has been found during lumbosacral joint extension in a cadaveric CT  
83 study.<sup>18</sup> Measurements of the parasagittal foramen area obtained at the entry, middle and exit  
84 zones via CT were used as a measure of success of endoscopic assisted lumbosacral  
85 foraminotomies in the dog.<sup>19</sup> In magnetic resonance imaging (MRI), features of DLSS are easily  
86 identified in dogs<sup>20</sup> and abnormal MRI findings are consistent with surgical findings.<sup>21</sup> Several  
87 studies have used MRI to measure different features regarding neural stenosis.<sup>4,22</sup> In two  
88 cadaveric dog studies it was shown that foraminal areas measured with CT<sup>18</sup> and MRI<sup>23</sup> were  
89 significantly different between flexed and extended lumbosacral positions.<sup>18,23</sup> The traditional  
90 imaging planes to investigate the spinal canal and the neuroforamina in magnetic resonance  
91 imaging are parasagittal, transverse (axial) and dorsal planes.<sup>4,20,21,24,25</sup> One study in dogs has  
92 investigated neuroforaminal dimensions and trajectories in the lumbosacral area with sagittal  
93 oblique images in computed tomography.<sup>18</sup> In humans, neuroforaminal dimensions are  
94 evaluated in standard parasagittal planes and image acquisition of the entry, middle and exit  
95 zones of the neuroforamina have been employed to subjectively assess L7 nerve root  
96 encroachment.<sup>26,27</sup> In a prospective human study it was suggested that coronal oblique lumbar  
97 MRI can precisely demonstrate nerve roots in foraminal and extraforaminal areas<sup>28</sup> and  
98 improve the diagnostic ability.<sup>29,30</sup>

99 Neither the effect of position of the lumbosacral spine nor the effect of a parasagittal oblique  
100 imaging plane on neuroforaminal measurements have been evaluated with magnetic resonance

101 imaging in dogs clinically affected by DLSS. The purpose of this study was to compare standard  
102 parasagittal foraminal measurements with those obtained in an oblique plane perpendicular to  
103 the exiting nerve root, that has been described in CT<sup>18</sup> in dogs. And secondly, to compare these  
104 measurements in both neutral and hyperextended positions of the lumbosacral area. Our null  
105 hypotheses were that 1) there is no difference between imaging planes and 2) there is no  
106 difference between lumbosacral position.

107

## 108 Materials and Methods

### 109 *Animals*

110 Thirty dogs, including agility, working and pet dogs, were prospectively recruited for this study  
111 between May 2010 and October 2012. They were all deemed to be clinically affected by  
112 lumbosacral disease and inclusion criteria were gait abnormalities, weakness or reluctance to  
113 jump, to rise or to exercise. The inclusion criteria were made selective for lumbosacral  
114 compromise, and pain on palpation of the dorsal lumbosacral area and pain on palpation of the  
115 sciatic outflow tract had to be present either as a separate expression of pain or in conjunction.  
116 All cases were examined by veterinarians at the clinic where the study was undertaken. General  
117 health of the dogs was within normal limits and other pelvic limb pathologies that could be the  
118 source of the reported clinical signs were excluded by palpation and range of motion  
119 examination of the pelvic limbs. For MRI, animals were placed under general anesthesia. They  
120 were induced with methadone (0.15-0.3mg/kg slow IV, Physeptone®, Martindale  
121 Pharmaceuticals, Harold Hill, Essex, UK), acepromazine (0.015-0.03mg/kg slow IV, Calmivet®,  
122 Vetoquinol, Lure Cedex, France) and propofol (4-6mg/kg IV, PropoFlo®, Abbott Laboratories,  
123 Maidenhead, Berkshire, UK) and maintained with isoflurane inhalation (IsoFlo®, Abbott  
124 Laboratories, Maidenhead, Berkshire, UK). After recovery from general anesthesia animals were  
125 discharged to their owners.

126

### 127 *Magnetic resonance imaging*

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128 For MRI examination, all patients were positioned head-first in dorsal recumbency. The neutral  
129 position was obtained with legs placed in natural flexed leg position and images were acquired  
130 utilising a table integrated spinal coil. For the hyperextended position legs were extended  
131 caudally and a flex array coil was used (Fig 1). Imaging was carried out on the same MRI system  
132 (Symphony Magnetom™ 1.5T, Siemens, Erlangen, Germany) using the routine protocol for spine  
133 investigation. The protocol consisted of the following sequences: standard sagittal T2-weighted  
134 (T2W) sequence (TR 3000ms, TE 101ms, FOV 360mm, matrix 512x448) with slice thicknesses  
135 of 2.3-2.5mm and a slice gap of 10%, dorsal STIR (TR 6000ms, TE 47ms, FOC 350mm, matrix  
136 384x270), transverse T2W (TR 3650ms, TE 99ms, FOV 200mm, matrix 394x270) and  
137 parasagittal oblique T2W (TR 2500ms, TE 105ms, FOV 220mm, matrix 320x232). The dorsal  
138 STIR and the transverse T2W sequences were not used in this specific study for data  
139 acquisition.

140 In hyperextended and neutral positions, and oblique and standard imaging planes, left and right  
141 foraminal apertures were evaluated for the entry, middle and exit zones of the nerve trajectory.  
142 The oblique parasagittal plane refers to a plane perpendicular to the nerve root, exiting the  
143 foramen. Fig. 2A indicates the trajectory of the L7 spinal nerve through the different zones of the  
144 neuroforamina. Parasagittal standard imaging planes are depicted to the left and parasagittal  
145 oblique to the right in the figures. The entrance zone is defined as the subarticular area medial  
146 to the pedicle, the middle zone is the area under the pars interarticularis and pedicle, and the  
147 exit zone represents the intervertebral foramen. Fig. 2B shows a T2W transverse image at the  
148 level of the lumbosacral junction with the corresponding parasagittal standard and oblique  
149 slices through the three different zones.

150 Foraminal areas in the three different zones were determined using the free-hand outline of the  
151 region of interest (ROI) using the integrated software image measurement tool of the MRI  
152 machine (Numaris4™ software, Siemens). The foraminal areas were measured by one  
153 investigator (JJ), a medical radiographer with extensive experience in MR imaging, in triplicate  
154 for each side in both planes and both positions. The measurements were displayed in cm<sup>2</sup> and  
155 averaged. Change in foraminal area was determined for neutral and hyperextended positions.

156 Examples of left and right entry, middle and exit zones on standard and oblique parasagittal  
157 image planes in neutral and hyperextended position are shown (Figs. 3-6).

158

### 159 *Statistical analysis*

160 Measurements were taken at each level of entry, middle and exit zones on both the left and  
161 right neuroforamina and were labelled as HS (hyperextended position standard plane), HO  
162 (hyperextended position oblique plane), NO (neutral position oblique plane) and NS (neutral  
163 position standard plane). A mixed-effects model was fit to all the area measurements where  
164 zone, plane, position and interactions, as well as the measurement side (L or R), were defined  
165 as fixed effects. Repeated measures were accounted for by specifying a random effect for  
166 each animal, and each zone within each animal, due to an observed interaction between zone  
167 and animal in the measured area. The response was transformed in order to ensure all  
168 modelling assumptions were satisfied. An ANOVA was performed on the final mixed-effects  
169 model to assess the significance of each of the zone, plane and position. The degrees of  
170 freedom in the ANOVA were estimated using the Satterthwaite approximation.<sup>31</sup> All  
171 hypothesis testing was undertaken at the 5% significance level. All analyses were conducted  
172 in the statistical software package R,<sup>32</sup> and the statistical tests were selected and performed by  
173 a statistician (DP) who is one of the authors.

174

### 175 Results

176 MRI images of lumbosacral foramina of thirty dogs included pure breed dogs (n=28) of nine  
177 breeds and cross breed dogs (n=2). Pure breed dogs were Border Collie (n=15), Labrador  
178 Retriever (n=4), German Shepherd Dog (n=2), Airdale Terrier (n=2), Pointer (n=1), Cocker  
179 Spaniel (n=1), Finnish Lapphund (n=1), Golden Retriever (n=1) and Lurcher (n=1). Sixteen  
180 female and 14 male dogs were part of the study. Dog ages ranged from 1.0 - 8.6 years (mean 4.7  
181 years). Body weights ranged from 8.2 – 49.5kg (mean 23.4kg).

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182 Four dogs (13.3%) only showed pain on palpation of the dorsal lumbosacral area (lumbosacral  
183 junction and/or spine) and four dogs (13.3%) only showed pain on palpation on the sciatic  
184 outflow tract, representing the major symptoms. Twenty-two dogs (73.4%) showed both of  
185 those signs combined. Of the 26 dogs (86.7%) showing pain on palpation of the sciatic outflow  
186 tract, eight of those dogs (30.8%) had unilateral signs. Additional clinical signs were: moderate  
187 partial to non-weight bearing lameness (n=16, 53.3%), stiffness (n=7, 23.3%), difficulties  
188 jumping or getting up (n=6, 20%), abnormal gait (n=3, 10%) crouched or haunched position  
189 (n=2, 6.7%), and weakness (n=2, 6.7%). Dogs could have more than one of the additional signs  
190 combined.

191 The mean and standard deviation values for foraminal area measurements are presented in  
192 Table 1 and 2, and results of the statistical comparisons for the variables are presented in Table  
193 3. The mixed effects model indicated that no significant difference was found between right and  
194 left foramina ( $p=0.1512$ ). The largest areas measured were the entry zone,  $0.53 \pm 0.09 \text{ cm}^2$   
195 (mean and SD), and the exit zone,  $0.55 \pm 0.13 \text{ cm}^2$  (mean and SD). The smallest area was the  
196 middle zone with  $0.42 \pm 0.07 \text{ cm}^2$  (mean and SD). The mixed effects model indicated a  
197 significant effect of each of zone, plane, and position ( $p<0.00005$ ). Measuring the entry or exit  
198 regions (rather than the middle region) both result in a significant increase in the measured  
199 area, on average ( $p<0.00005$ ). Measurement in the standard plane (as opposed in the oblique  
200 plane), results in a significant increase in the mean measurement ( $p<0.00005$ ), revealing that  
201 the neuroforaminal area acquired using oblique sagittal planes (NO, HO) was significantly  
202 smaller than measurements in the standard parasagittal plane (NS, HS), except for the  
203 hyperextended position in the middle and exit zone and the neutral position in the middle zone  
204 of the right foramina (Fig. 7, Table 1 - 3). Comparing the influences of the two different positions  
205 of the lumbosacral area, the neuroforaminal areas acquired with hyperextended positions were  
206 significantly smaller ( $p<0.0001$ ) than measurements acquired in the neutral position - in the  
207 corresponding standard parasagittal plane (HS compared to NS) as well as the oblique  
208 parasagittal plane (HO compared to HS) (Fig. 3 - 6). Furthermore, there is a significant  
209 interaction between zone and plane. Specifically, compared to the middle zone and oblique  
210 plane, both entry and exit zones in the standard plane result in an increase in area, however

211 only entry is significant ( $p=0.0034$  and  $p=0.7755$ ) and the statistical difference was most  
212 pronounced for neuroforaminal dimensions evaluated in the oblique plane and hyperextended  
213 position (Fig. 3 and Fig. 5). There is a significant interaction between all of zone, plane and  
214 position ( $p = 0.0235$ , Table 3). Thus, on average, the minimal measurement area is predicted to  
215 be for the middle zone, for a dog in the hyperextended position, observed in the oblique  
216 parasagittal plane. No other lesions were found on MRI examination which might account for  
217 the reported clinical signs.

218

## 219 Discussion

220 Magnetic resonance imaging is a widely used advanced imaging modality to confirm the  
221 diagnosis of DLSS in dogs.<sup>20</sup> In the present study standard parasagittal MRI foraminal  
222 measurements at the level of the lumbosacral junction were compared with those obtained in a  
223 novel oblique plane perpendicular to the exiting nerve root. The mixed-effect model indicates  
224 that the neuroforaminal areas acquired using oblique sagittal planes were smaller, on average,  
225 compared to the standard plane. Furthermore, measurements in both the neutral and  
226 hyperextended positions of the lumbosacral area revealed that the neuroforaminal area was, on  
227 average, significantly smaller in the hyperextended position.

228 Standard parasagittal plane in MRI imaging is well established to investigate the spinal canal  
229 and the neuroforamina in humans, and one study concluded that the appropriate use of oblique  
230 section selections in human MRI can improve diagnostic capability.<sup>29</sup> Excellent visualisation of  
231 nerve roots and foramina with oblique imaging planes in the cervical spine was reported.<sup>33</sup> The  
232 relationship of nerve roots and foramina to intraforaminal structures and the boundary of the  
233 foramina can be determined including the intraforaminal fat signal.<sup>34</sup> Several studies  
234 investigating the diagnostic value of angled sagittal MRI in the cervical spine have been pursued  
235 in humans and oblique imaging has been found to be a more accurate test compared to  
236 conventional parasagittal planes.<sup>35</sup> The results of the present study reveal that the  
237 neuroforamina area acquired using oblique planar images was smaller than standard  
238 parasagittal measurements with the middle zone being the narrowest. These results are in

239 agreement with those of an earlier study using CT which investigated neuroforaminal  
240 dimensions and trajectories in the lumbosacral area using sagittal oblique images in dogs and  
241 found that the middle and exit zones had much smaller cross-sectional areas.<sup>18</sup> It was concluded  
242 in their study that oblique planes provided images in which the lumbosacral intervertebral  
243 foramen is visualized at its smallest cross section and thus the L7 nerve is visualized in true  
244 cross section. As compression of the L7 nerve within the lumbosacral intervertebral foramen  
245 may be more likely to occur at the point at which the cross-sectional area of the foramen is  
246 smallest, this imaging plane may potentially provide increased sensitivity in the diagnosis of  
247 lumbosacral foraminal stenosis and nerve root compression. Similar results were obtained in  
248 studies investigating oblique planes in the cervical spine in humans.<sup>36</sup> As the dimensions of the  
249 foramina are of clinical importance in the diagnosis of foraminal stenosis and radiculopathy, it is  
250 recommended in humans to add oblique MRI when the clinical exam is suggestive for  
251 radiculopathy in the cervical spine because the oblique images provide data not available from  
252 the conventional parasagittal acquisition technique. A significant correlation using MRI and CT  
253 on human cadaveric cervical spines between nerve root compression and decreased foraminal  
254 area was found which might help in the diagnosis of foraminal stenosis.<sup>30</sup> In another study it  
255 was concluded that angled cervical MRI provides statistically significant increase in specificity  
256 and accuracy of diagnosing foraminal stenosis, providing a clearer view of certain anatomic  
257 structures because the imaging plane is oriented perpendicular to the true course of the neural  
258 foramina and facilitates the identification of diseases, especially laterally.<sup>35</sup> In other studies in  
259 humans it was found that the oblique view added important information not available on the  
260 sagittal images or clarified changes seen on the axial images of cervical spine MRI.<sup>37</sup> The fact  
261 that diminished foraminal area is evident more pronouncedly on oblique planar image  
262 acquisition in the present study suggests that this novel plane could be used as a useful imaging  
263 tool to interrogate L7 nerve root encroachment.

264 Neurogenic claudication defined by intermittent pain or paresthesia in the legs in humans is  
265 brought on by walking and standing and relieved by sitting or lying.<sup>10</sup> In dogs with lumbosacral  
266 degenerative disease certain movements are more painful than others.<sup>4,5-8</sup> In the present study,  
267 foraminal apertures in the lumbosacral area revealed significant differences between

268 hyperextended and neutral patient positioning. Neuroforaminal dimensions in the  
269 hyperextended position were significantly smaller than in the neutral position. Thus, decreased  
270 foraminal dimensions may increase compression on neural structures embedded in the  
271 intervertebral foramen depending on lumbosacral vertebral position. This may occur when  
272 dogs are jumping over an agility course jump, into the owners' car, onto a sofa, when going up  
273 stairs, or when getting up after lying down in a curled-up position for a prolonged period, all of  
274 which are common observations in dogs affected by DLSS. Nerve root compression in the  
275 foramen occurs by facet subluxation with associated bulging of the posteroinferior portion of  
276 the ligamentum flavum and posterior/dorsal bulging of the intervertebral disc.<sup>5</sup> With regard to  
277 foraminal size, human studies have shown that dimensions of the neural foramina are position  
278 dependent.<sup>11,38</sup> Position-dependent changes in relationship of the nerve root with the adjacent  
279 disk were frequently found and change in pain score was most closely associated with foraminal  
280 changes.<sup>11</sup> Comparing recumbant, upright weight-bearing and dynamic-kinetic spinal imaging it  
281 was found that a greater degree of neural foraminal stenosis occurs in extension while flexion  
282 leads to lessening and resolution of narrowing.<sup>17</sup> Dynamic changes in L7-S1 intervertebral  
283 foraminal morphology have been found in dogs with lumbosacral disease with positional  
284 computed tomography<sup>17</sup>, detecting a significant decrease in mean foraminal area for position in  
285 extension versus flexion. The absolute numbers of foraminal area measurement in extended  
286 position were much smaller compared to the values we retrieved in our study. This might be  
287 explained by the fact that the lumbosacral area was positioned in a extreme extended  
288 positioning in the mentioned study<sup>17</sup> and in a more normal position in our study. Conducting a  
289 CT study with cadaveric dogs it was found that the lumbosacral intervertebral foraminal area  
290 was smaller when the lumbosacral junction was extended, rather than flexed.<sup>18</sup> The significant  
291 effect of patient positioning on neuroforaminal dimension provides corroborative evidence that  
292 spinal position may influence neural claudication in clinically affected patients. In the  
293 mentioned study the middle and exit zones had much smaller cross-sectional areas compared  
294 with that of the entrance zone.<sup>18</sup> This is confirmed partly in our study where the middle zone  
295 has the smallest cross-sectional area in both planes and both lumbosacral positions, being more  
296 likely to be the site of compression. The exit zone in our study was smaller than the entrance  
297 zone in the hyperextended position but larger than the entrance zone in the neutral position.

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298 This might be an indication that in the hyperextended position there is more dynamic  
299 compression of the exit zone due to anatomical change regarding positioning of ligaments and  
300 bulging of the intervertebral disc, compared to the entry zone, which is characterized by a more  
301 bony anatomy than soft tissue anatomy.

302 We found the same percentage of both genders to be affected by symptoms of DLSS, in contrast  
303 to other studies<sup>39</sup> where males were overrepresented. This might just be coincidence. Working  
304 dogs like the Huntaway have been reported to be over-represented regarding DLSS in New  
305 Zealand,<sup>40</sup> while the Border Collie was the main affected breed in the present study and a  
306 previous study.<sup>39</sup> Most dogs affected by DLSS exhibit pain and sensory dysfunction with few  
307 showing motor deficits.<sup>41,42</sup> Pain represents the predominant clinical sign followed by lameness,  
308 stiffness and difficulties jumping, which is also the case for the present study.<sup>41,42</sup> In one third of  
309 dogs in our study signs were unilateral and yet there was no significant difference of  
310 neuroforaminal dimension detected between left and right. This may point toward clinical signs  
311 not necessarily being correlated with the dimension of the intervertebral foramina measured on  
312 MRI. Other studies also observed that imaging findings do not always correlate well with clinical  
313 signs.<sup>24</sup> A recent study which quantified foraminal area in dogs affected by DLSS did not reveal a  
314 direct correlation between foraminal area and clinical signs.<sup>17</sup> Further studies are needed to  
315 investigate the relationship between clinical signs, especially dynamic movements, and MRI  
316 findings in large numbers of clinical cases. We submit that the new parasagittal oblique plane  
317 described here may be a useful diagnostic plane to diagnose foraminal stenosis more reliably,  
318 but this remains to be seen in consecutive studies.

319 CT is a very sensitive diagnostic imaging tool for bony changes and MRI is considered to be  
320 more sensitive for detection of soft tissue changes. The step window display facilitated  
321 discrimination of bone margins for most dogs, however also created difficulties in assessing  
322 bone margins.<sup>17</sup> Epidural fat surrounds the cauda equina nerve roots and provides a natural  
323 source of soft tissue contrast in normal dogs.<sup>43</sup> In dogs with lumbosacral stenosis, however,  
324 epidural fat is usually lost at sites of cauda equina compression. Contrast-enhanced CT has a  
325 positive-predictive value of 81% for compressive soft tissues involving the lateral recesses in  
326 dogs with lumbosacral stenosis.<sup>44</sup> In MRI, however, compression of the nerve roots by

327 protruding disc material and loss of epidural fat is easily identified.<sup>11,20</sup> T1W sagittal images  
328 were found most useful in imaging the cross sectional area of the intervertebral canal and in  
329 demonstrating foraminal narrowing.<sup>21</sup> In the present study T2W images were chosen as the  
330 sequence to evaluate the images because the T2W images are one of the most frequently used  
331 sequences by clinicians for diagnostic purposes in a clinical setting and our objective was to  
332 provide maximal applicability to typical clinical scenarios. Together with T1W, the T2W  
333 sequence has been used in canine and human studies to diagnose foraminal stenosis.<sup>28,42</sup>  
334 Foraminal area with reconstructed sagittal oblique CT images was investigated by angulating  
335 standard sagittal images perpendicular to the transverse plane angle.<sup>18</sup> Using MRI, sagittal plane  
336 images do not need to be reconstructed as in CT and are valuable in demonstrating foraminal  
337 disc protrusion and associated foraminal stenosis with a clear advantage over CT imaging.<sup>21</sup>  
338 Freehand tracing around the margins of the foramen to quantify the foraminal area has been  
339 undertaken in dogs using CT images.<sup>17,19</sup> Because this process may be inaccurate implicating  
340 errors in positioning the cursor and in accurately defining the boundaries of the foramen, in a  
341 recent study it was attempted to improve boundary detection with modeling the soft tissue  
342 component by injecting a plastic material into the foramen of the study cadavers.<sup>18</sup> In the  
343 present study foraminal areas were determined using the free-hand outline of the region of  
344 interest using the epidural fat as a border for the outline of the foraminal boundaries. We accept  
345 the limitation that there is still a risk of under- or overestimation of the foraminal area and  
346 further studies including evaluation of inter- and intraobserver variability are warranted.

347 A second limitation of our study is that to simulate the dynamics of the lumbosacral junction the  
348 normal position was compared with the hyperextended position and not with a hyperflexed  
349 position. To investigate and demonstrate more extreme changes of foraminal dimensions under  
350 the influence of position of the lumbosacral junction, a hyperflexed position may be used in  
351 further studies. A third limitation of this study is slice thickness, which varied according to the  
352 size of the patient. We used the thickest slice size possible to minimize artifact but in some  
353 patients the slice thickness was decreased in order to relate the slices definitively to the planes  
354 of the entry, middle and exit zones. Additional limitations of the study is the lack of a group of  
355 painfree dogs with similar signalement and without any clinical signs of lumbosacral disease as

356 controls and the retrospective nature of the study. The inclusion criteria were made selective  
357 for lumbosacral compromise, but inherently in a retrospective study we are limited by the  
358 histories and exam findings recorded in the medical records, by several different clinicians.  
359 Besides many different nonspecific clinical signs, that can be attributed to several pelvic limb  
360 pathologies, the clinical sign all those dogs had in common was lumbosacral pain - on dorsal  
361 palpation of the lumbosacral area or pain on palpation of the sciatic outflow tract, either as a  
362 separate expression of pain or in conjunction. Despite the often nonspecific clinical signs of  
363 degenerative lumbosacral stenosis, lumbosacral pain is considered the most consistent clinical  
364 finding.<sup>45</sup> Lumbosacral pain can be elicited specifically by dorsal palpation of the lumbosacral  
365 area<sup>45</sup> and the sciatic outflow tract.<sup>1</sup> We considered this specific pain responses as a strong  
366 indicator for a pathology of the lumbosacral area. It is the standard of care and medical record  
367 documentation in the clinic where the study took place, that exclusion of mention of other pelvic  
368 limb lesions in the medical records indicated that the examining clinicians have excluded other  
369 etiologies. Being also part of the inherent limitation of a retrospective study, we therefore made  
370 the assumption that no other pelvic limb pathologies have been detected in the presented dogs  
371 with the assumption that the pelvic limbs were examined by widely accepted good general  
372 practice and with consistent clinical exam. There is a lack of gold standard in this study  
373 population, however using what has been published in the literature yields to us a valid form of  
374 "reference standard". The goals and results of this study are not intended to correlate the  
375 clinical signs to MRI findings. Clinical signs were intended to define inclusion criteria to create a  
376 study population with clinical signs most representative of lumbosacral pathology.

377 Notwithstanding the limitations of our study, we conclude that the parasagittal oblique plane  
378 may represent a potentially more accurate objective measure of L7 neuroforaminal dimensions.  
379 Furthermore, we have shown that spinal position may influence dimensions of neuroforamina  
380 as detected by MRI in clinically affected patients and that positional MRI is a feasible technique  
381 for quantifying dynamic changes in L7-S1 foraminal morphology. Authors propose that  
382 positional MRI with parasagittal oblique image acquisition should form part of any imaging  
383 interrogation of patients with clinical signs likely attributable to DLSS, particularly where  
384 conventional imaging parameters may prove inconclusive. Further application of these

385 techniques in larger case numbers, cohort studies, anatomical comparative studies and surgical  
386 confirmation of imaging findings will all be required to further establish applicability of our  
387 findings.

388

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543

544 Table 1. Measured Area of Left Neuroforamina in Normal Position Standard Plane, Normal  
545 Position Oblique Plane, Hyperextended Position Standard Plane and Hyperextended Position  
546 Oblique Plane, Comparing Entry, Middle and Exit Zone (n=30)

547

548 Entry Middle Exit

549

550 Mean SD Mean SD Mean SD

551 (cm<sup>2</sup>) (cm<sup>2</sup>) (cm<sup>2</sup>)

552

553 HS 0.55 0.13 0.38 0.10 0.48 0.17

554 HO 0.43 0.10 0.34 0.07 0.42 0.13

555 NS 0.64 0.18 0.54 0.15 0.72 0.21

556 NO 0.54 0.11 0.45 0.09 0.58 0.21

557

558 NS = normal position standard plane, NO = normal position oblique plane, HS = hyperextended  
559 position standard plane, HO = hyperextended position oblique plane

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566 Table 2. Measured Area of Right Neuroforamina in Normal Position Standard Plane, Normal  
567 Position Oblique Plane, Hyperextended Position Standard Plane and Hyperextended Position  
568 Oblique Plane, Comparing Entry, Middle and Exit Zone (n=30)

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	Entry		Middle		Exit	
	Mean	SD	Mean	SD	Mean	SD
	(cm <sup>2</sup> )		(cm <sup>2</sup> )		(cm <sup>2</sup> )	
HS	0.53	0.14	0.37	0.09	0.46	0.16
HO	0.43	0.10	0.34	0.09	0.44	0.15
NS	0.64	0.15	0.49	0.11	0.73	0.19
NO	0.51	0.10	0.45	0.11	0.57	0.21

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580 NS = normal position standard plane, NO = normal position oblique plane, HS = hyperextended  
581 position standard plane, HO = hyperextended position oblique plane

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584 Table 3. Results of the ANOVA, Demonstrating the Statistical Significance of Each Variable\*

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	F-value	P-value
Side	2.0646	0.1512
Zone	40.0215	<0.00005
Plane	125.2637	<0.00005
Position	384.4908	<0.00005
Zone:plane	4.2470	0.0147
Zone:position	13.9338	<0.00005
Plane:position	2.8302	0.0930
Zone:plane:position	3.7742	0.0235

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599 \*The ANOVA indicates that each zone, plane, position, the two-way interaction between zone  
600 and plane, and zone and position, and the three-way interaction between zone, plane and  
601 position, all have a significant effect on the measured neuroforaminal area.

602

603

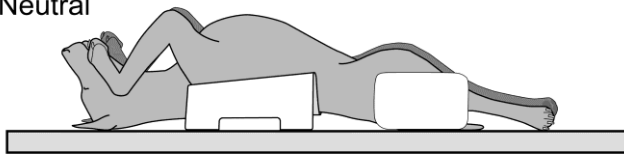
604

605 Figure legends

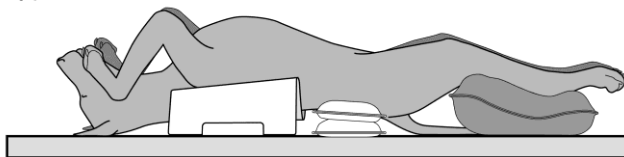
606

607 FIG. 1. Schematic drawings of positioning of the dogs for MRI. Neutral position was obtained  
608 with legs placed in natural flexed frog-leg position, with foam wedges placed under the distal  
609 femur/stifle area if necessary, to keep the pelvic limbs balanced. Hyperextended position was  
610 obtained with legs extended caudally to extend the hip joint, with both femora affixed parallel to  
611 each other, and elevating the lumbosacral area with sandbags.

Neutral



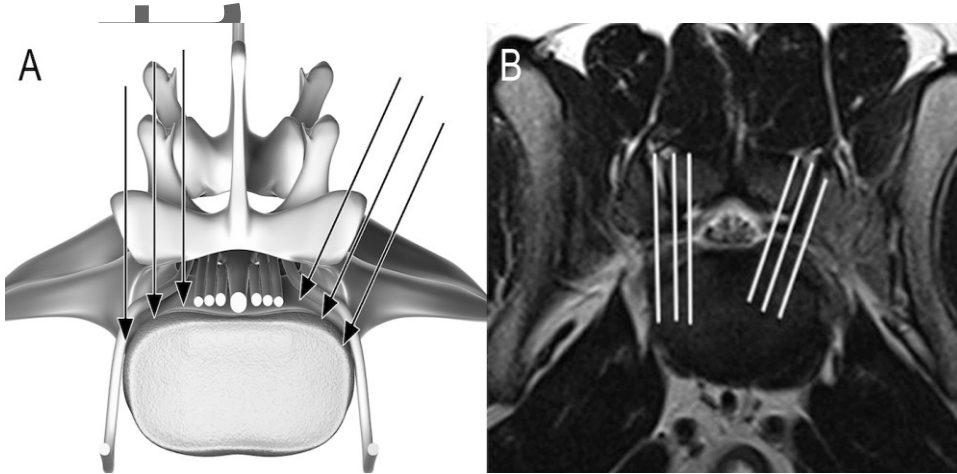
Hyperextended



612

613 FIG. 2. Schematic drawing (A) and T2W transverse MRI image (B) at the level of the lumbosacral  
614 junction indicating the trajectory of the L7 spinal nerve through the different zones of the  
615 intervertebral neuroforamina. Parasagittal standard imaging planes are depicted to the left and

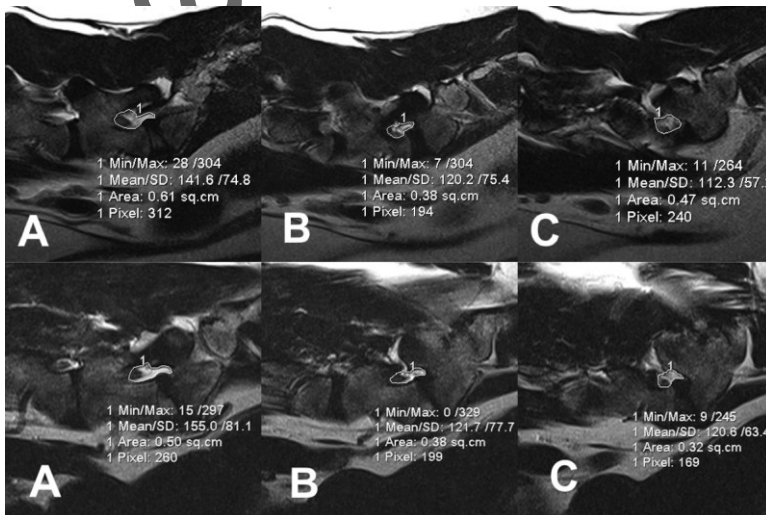
616 oblique imaging planes to the right in the drawing and the image. Entry, middle and exit zones  
 617 are represented from axial to abaxial by sequential arrows on image A and by lines on image B.



618

619 FIG. 3-6. Zone measurements as region of interest (ROI) of the foraminal aperture in the entry  
 620 (A), middle (B) and exit (C) zone in the parasagittal plane (T2W).

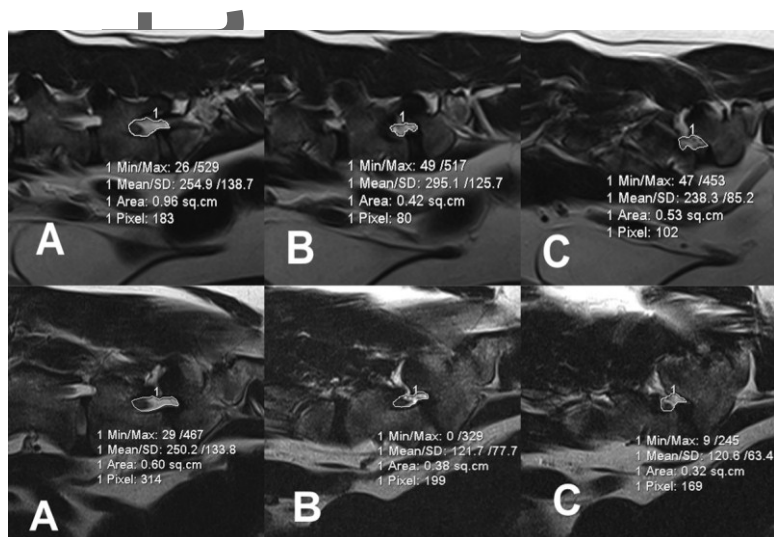
621 FIG. 3. Left standard (first row) and oblique (second row) parasagittal image planes in  
 622 hyperextended position of the lumbosacral area.



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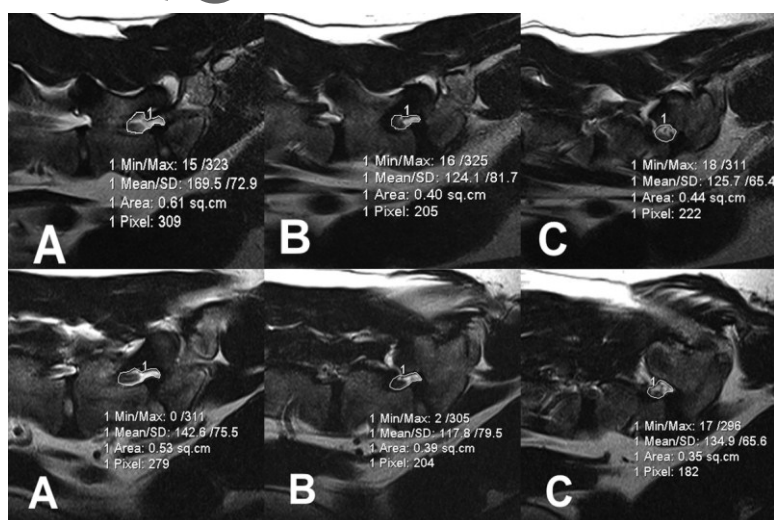
625 FIG. 4. Left standard (first row) and oblique (second row) parasagittal image planes in neutral  
626 position of the lumbosacral area.



627

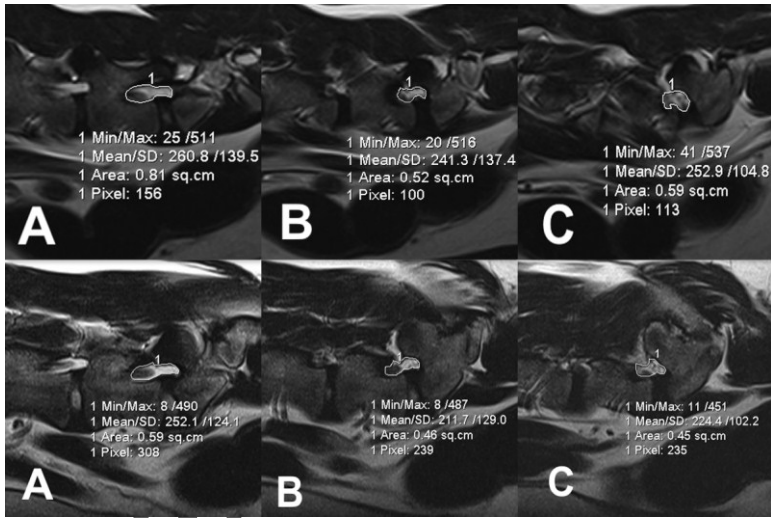
628

629 FIG. 5. Right standard (first row) and oblique (second row) parasagittal image planes in  
630 hyperextended position of the lumbosacral area.



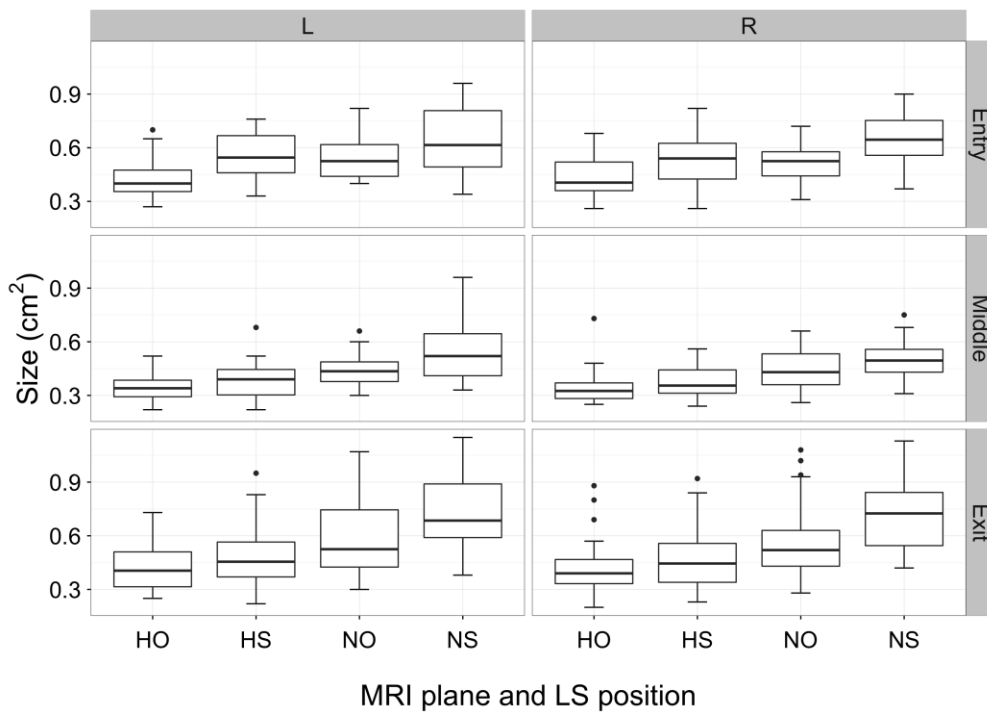
631

632 FIG. 6. Right standard (first row) and oblique (second row) parasagittal image planes in neutral  
633 position of the lumbosacral area.



634

635 FIG. 7. Box and whisker plot of data from area measurements of the left (L) and right (R)  
 636 middle and exit zones of neuroforamina (cm<sup>2</sup>) comparing two MRI views and two positions of  
 637 the lumbosacral (LS) area (HS–hyperextended position standard plane, HO–hyperextended  
 638 position oblique plane, NO–neutral position oblique plane, NS–neutral position standard plane).



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